

FPGA implementation of fractal patterns classifier for multiple cardiac arrhythmias detection

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ABSTRACT

This paper proposes the fractal patterns classifier for multiple cardiac arrhythmias on field-programmable gate array (FPGA) device. Fractal dimension transformation (FDT) is employed to adjoin the fractal features of QRS-complex, including the supraventricular ectopic beat, bundle branch ectopic beat, and ventricular ectopic beat. FDT with fractal dimension (FD) is addressed for constructing various symptomatic patterns, which can produce family functions and enhance features, making clear differences between normal and unhealthy subjects. The probabilistic neural network (PNN) is proposed for recognizing multiple cardiac arrhythmias. Numerical experiments verify the efficiency and higher accuracy with the software simulation in order to formulate the mathematical model logical circuits. FDT results in data self-similarity for the same arrhythmia category, the number of dataset requirement and PNN architecture can be reduced. Its simplified model can be easily embedded in the FPGA chip. The prototype classifier is tested using the MIT-BIH arrhythmia database, and the tests reveal its practicality for monitoring ECG signals.

Keywords: Field-Programmable Gate Array (FPGA); Fractal Dimension Transformation (FDT); Fractal Dimension (FD); Probabilistic Neural Network (PNN)

1. INTRODUCTION

The electrocardiogram (ECG) signal can be measured non-invasively by placing electrodes on the body surface that provides information of myocardium electric activity and heart physiological function. An ECG signal shows as an almost periodic signal, and can reveal symptomatic information in the dysfunction duration. Currently, portable and stationary monitoring devices have been used on healthcare systems. Holter recorder is a well-known portable device and used to record the electrical activity with surface electrodes placed on the chest. However, its diagnostics is off-line analysis from the recorded data,

and uses a cardiogram to identify arrhythmic types of the patients. Stationary monitors, such as dedicated or PC-based devices, have also been used on healthcare systems, which results in expensive solutions and limiting the portability [1,2]. Since telemedicine has also been used to acquire patient's information, and has portable configuration for patient monitoring in remote non-clinical environments, it can be used in home healthcare, elder communities, and public place to acquire patient's information. It has become a commonly used technology due to its low-cost, compactness, and short design-cycle. This remote device is an embedded hardware with FPGA, Bluetooth, RFID, and Zigbee. Via wireless transmission between the biosensor and supervision device, FPGA makes the ECG signal processing and sends digital signal to a remote monitor [3]. For a portable monitor design, FPGA device provides a promising solution to hardware implements.

FPGA device provides the flexibility and potential alternative to design hardware, including built-in DSP, analog and digital I/O, signal generation, communication, and specific functions for signal processing and controllers. It has been applied for digital filters design [4,5], signal analysis and classification [6,7], fault detection [8], and Fuzzy logic controller [9]. For signal analysis, transform methods have been used to extract features in the transform domain, such as fast Fourier transform (FFT) and wavelet transform (WT). However, the FFT technique is limited by the processing time, computational complexity, and the number of samples. The more samples, the more accurate parameters will be estimated. It will increase the memory requirement. WT can be chosen with a very desirable frequency and time characteristics, allowing the visualization with the short/broad window at the high/low frequencies. It is a dilated or constricted function by changing dilation and translation coefficients for feature extraction. WT process uses a several-structured filter bank to generalize several frequency bands containing decomposed signals [6,7]. Significant features are obtained at specific wavelet coefficients with a trial procedure of wavelet decomposition and experiences.

To overcome the drawbacks, an iterated function system (IFS) is proposed for modeling the non-linear interpolation function [10-14]. Its modification, the so-called FDT function, is simple in form and consists of sinusoidal terms to the affine maps, making the model more flexible for processing irregular signals. FDT functions with FD are used to construct the fractal patterns from ECG signals in the time-domain, including the “Q-R Segment” and “R-S Segment”. The transform method results in data self-similarity and enhances the features for the same category. The PNN-based classifier is developed to perform the classification tasks. The performance of this method is presented and promising results are given for classification applications, such as the straightforward mathematical operation, flexible pattern mechanism, and high tolerance capability [15-17]. These algorithms can be easily programmed into the FPGA chip. The FPGA device has an inherent parallel architecture allowing designers to execute the multiple inputs and control loops simultaneously without slowing down the execution time and applications. From the test results, they appear to be computationally efficient and accurately recognize for patterns classification.

2. MATHEMATICAL BACKGROUND

2.1. Fractal Dimension Transformation (FDT)

An IFS has been proposed for image compression and signal modeling, and is capable of producing family functions with different fractal dimensions (FDs). It is a finite set for contraction mappings, and has been used to create images, various waveforms and patterns for medical image classification and biomedical signal analysis [10,11]. IFS is implemented with similarity maps, and the resulting data are self-similar. The significant removal of redundancy is related to the self-similarity of natural patterns. In modeling the pattern of a function or data sequence $x[t]$, $t = 1, 2, 3, \dots, N$, the p th interpolation map W_p , $p = 1, 2, 3, \dots, P$, can be presented as

$$W_p \left(\begin{bmatrix} t \\ x[t] \end{bmatrix} \right) = \begin{bmatrix} a_p & b_p \\ c_p & d_p \end{bmatrix} \begin{bmatrix} t \\ x[t] \end{bmatrix} + \begin{bmatrix} e_p \\ f_p \end{bmatrix} \quad (1)$$

$$\begin{cases} W_p(t) = a_p t + b_p x[t] + e_p \\ W_{px}(x[t]) = c_p t + d_p x[t] + f_p \end{cases} \quad (2)$$

For each map, W_p maps the data sequence $x_p[t]$ onto the subsequences with N_p sampling data in the interval $[N_{p1}, N_{p2}]$, and the maps can be constructed side by side. The remaining map parameters c_p , d_p , and f_p can be solved by minimizing the sum of squared errors between the transformed data and the original data in the range of the p th map, and can be justified by the Collage Theorem [12,13]:

$$e_p = \sum_{t=N_{p1}}^{N_{p2}} \left(W_{px}(x_p[t]) - x_p[t] \right)^2 \quad (3)$$

where $n = \text{int} \left[\left(\frac{t - N_{p1}}{N_{p2} - N_{p1}} \right) (N - 1) \right]$, $N_p = N_{p2} - N_{p1} + 1$,

and $N = N_1 + N_2 + N_3 + \dots + N_p + \dots + N_P$. To improve the constraint, non-linear interpolation is used to adjoin the data among the interpolation points, which makes the model more flexible for processing non-linear and irregular signals. Non-linear terms as sinusoidal functions can be added to W_p . The non-linear interpolation function can be represented as

$$W_{px}(x_p[t]) = c_p n + d_p x_p[t] + f_p + g_p \sin \left(\frac{\pi n}{N} \right) \quad (4)$$

A fractal pattern of ECG signal can be adjoined with several segments such as P-R interval, P-R segment, Q-R-S complex, S-T segment, or Q-T interval. The non-linear function with fractal dimension (FD) will change the ECG signals into fractal patterns at different scale parameters. FD must be a parameter between 1 and 2 for processing one-dimensional signals. The non-linear interpolation function, FDT with FD, can be modified as

$$\phi_{pt}(x_p[t]) = c_p n' + d_p x_p[t] + f_p + g_p \sin \left(\frac{\pi n'}{D} \right) \quad (5)$$

$$n' = \left(\frac{D - 1}{N_p - 1} \right) t \quad (6)$$

where D is a FD parameter ($1 < D < 2$). The remaining map parameters c_p , d_p , f_p , and g_p can be solved by

$$\sum_{t=1}^{N_p} \begin{bmatrix} S_t \cdot S_t^T \\ d_p \\ f_p \\ g_p \end{bmatrix} = \sum_{t=1}^{N_p} S_t \cdot x_p[t] \quad (7)$$

$$S_t = \begin{bmatrix} n' & x_p[t] & 1 & \sin \left(\frac{\pi n'}{D} \right) \end{bmatrix}^T \quad (8)$$

Apply sequence data $x_p[t]$ are the sampling data from the ECG signals. The fractal patterns can be reconstructed as [14]

$$\Phi(\phi_{pt}) = \bigcup_{p=1}^P \phi_{pt}(x_p[t]) \quad t = 1, 2, 3, \dots, N_p \quad (9)$$

Equations (5) and (6) are used to extract the features from the ECG signals, and Equation (9) is utilized to construct the fractal patterns of cardiac arrhythmias.

2.2. Artificial Neural Network (ANN)

The PNN consists of four layers, including the input layer, hidden layer, summation layer, and output layer, that

has the parallelism distributed process, learning, and pattern recognition ability. In this study, we have considered the sequence data $x_p[t]$, $t=1, 2, 3, \dots, N_p$, with P segments from the ECG signal, and a fractal pattern Φ can be represented as

$$\Phi = \left[\varphi_{11}, \varphi_{12}, \varphi_{13}, \dots, \varphi_{1N_1} \mid \varphi_{21}, \varphi_{22}, \varphi_{23}, \dots, \varphi_{2N_2} \mid \dots \mid \varphi_{P1}, \varphi_{P2}, \varphi_{P3}, \dots, \varphi_{PN_P} \right] = \bigcup_{p=1}^P \varphi_{pi} (x_p [t]) \quad (10)$$

The vector Φ can be also combined as $\Phi = [\varphi_{11}, \varphi_{12}, \varphi_{13}, \dots, \varphi_{1N_1} \mid \varphi_{21}, \varphi_{22}, \varphi_{23}, \dots, \varphi_{2N_2} \mid \dots \mid \varphi_{P1}, \varphi_{P2}, \varphi_{P3}, \dots, \varphi_{PN_P}] = [\phi_1, \phi_2, \phi_3, \dots, \phi_i, \dots, \phi_N]$, $i = 1, 2, 3, \dots, N$, $N = N_1 + N_2 + N_3 + \dots + N_p$, and each feature ϕ_i is connected to the input nodes of input layer. The number of input nodes is equal to the number N . The number of hidden nodes H_k ($k = 1, 2, 3, \dots, K$) is equal to the number of training data, while the number of summation nodes S_j and output nodes O_j ($j = 1, 2, 3, \dots, m$) equals to the types of cardiac arrhythmias. Therefore, its architecture can be easily to determined without any trial-and-error procedure. The weights w_{ki}^{IH} (connecting the k th hidden node and the i th input node) and w_{jk}^{HS} (connecting the j th summation node and the k th hidden node) are determined by K input-output training pairs. In the hidden node, a normalized Gaussian function H_k is applied to the Euclidean distance E_d between the unknown pattern Φ and K training patterns w_{ki}^{IH} . The function H_k is inversely proportional to the distance E_d . If E_d approaches zero, the unknown pattern Φ is similar to any training data. This concept can be used for analyzing pattern relations. The output O_j can be computed by

$$H_k = \exp \left[-\sum_{i=1}^N \frac{(\phi_i - w_{ki}^{IH})^2}{2\sigma_k^2} \right] = \exp \left[-\frac{E_d^2}{2\sigma_k^2} \right] \quad (11)$$

$$O_j = \frac{\sum_{k=1}^K w_{jk}^{HS} H_k}{\sum_{k=1}^K H_k} \quad j = 1, 2, 3, \dots, m \quad (12)$$

where the weights w_{ki}^{IH} are created by training data $\Phi(k) = [\phi_1(k), \phi_2(k), \phi_3(k), \dots, \phi_N(k)]$, $k=1, 2, 3, \dots, k, \dots, K$; the weights w_{jk}^{HS} are the desired outputs associated with each stored pattern w_{ki}^{IH} . The value of w_{jk}^{HS} will be equal to “1” or “0”. The value will be set to be “1” when the k th training data belonged to the j th class; σ_k is the smoothing parameter. Finally, the maximum output $O_{\max} = [O_1, O_2, O_3, \dots, O_j, \dots, O_m]$ indicates the type of cardiac arrhythmias.

In Equation (11), the smoothing parameter $\sigma_1 = \sigma_2 = \sigma_3 = \dots = \sigma_K = \sigma$ ($\sigma \neq 0$) would refine the classification accuracy. The non-linear optimization method, such as gradient descent method, steepest descent method or New-

ton-Raphson method [15-17], is employed to adjust the parameter σ and minimize the error with iteration procedures. It is intended to minimize the predicted squared error function $e_j(q) = [T_j - O_j(q)]^2$, and is updated by using pattern learning as

$$\sigma(q+1) = \sigma(q) + \eta \frac{\partial e_j(q)}{\partial \sigma} \quad (13)$$

where T_j is the desired output for training pattern $\Phi(k)$, η is the learning rate, and q is the iteration number. The PNN based classifier has a dynamic and fast adaptation ability with continuity add-in or delete-off training data by automatically tuning the desired outputs and parameters σ of hidden nodes.

3. FPGA IMPLEMENTATION

3.1. FPGA Development Environment

The field-programmable gate array (FPGA) is a semiconductor device that can be configured by the customer or the designer after manufacturing. It has the array architecture of logical elements, which can be used to design any logical functions to implement the given applications, such as an application-specific integrated circuit (ASIC). FPGA is also a programmability device, like programmable ROMs, and its programming techniques include antifuse-based device (Programmed Once) and static-memory-based device (Reprogrammed an Unlimited Number of Times). A typical FPGA consists of configurable logic blocks (CLB), input/output blocks (IOB), and programmable interconnects [4-9]. Each CLB can design the logical functions and latching data with combinational logic and sequential logic (AND, OR, Flip-flops, and Registers). IOBs provide the interface between external pins and internal logics. Programmable interconnects link the CLBs, I/O pins, and other resources on-chip memory through the routing paths, where interconnection among these blocks can be programmed by using hardware description language (HDL). Then, the designs can transferred the descriptions to gate-level netlists and dataflow on a chip. The prototype device can be implemented, tested, debugged, and modified as needed in a short design cycle.

Custom-design platforms have been provided to the FPGA implementation, such as Verilog, ModelSim, and Quartus II, and its development environment can simulate and verify the logic designs before initiating the compilation process [18-20]. However, HDL is a low level text-based programming language used for FPGA hardware design. Currently, LabVIEW extends the graphical programming tools to FPGA-based hardware. It has parallel execution, data acquisition, and floating-point arithmetic (Data Word Length: 8, 16, and 32 bit) functions to proc-

ess signals on FPGA, and embeds specific functions for math, signal analysis/generation, comparison logic, linear/non-linear control, analog and digital I/O, and timing. In this workspace, designers can quickly develop specific and reliable embedded systems containing FPGA-chips, real-time processor, and human machine interface (HMI). Graphical user interface for windows application has shorter design cycle, reprogrammability, and flexibility, which is much better than text-based languages. Under this development environment, we use saturation arithmetic functions to configure the combinational logics without prior complex digital design or electronic design automation (EDA) tools, and then to embed intelligent algorithms on the compact chip.

3.2. FDT Implementation with FPGA

An ECG signal is measured with the modified limb lead II (ML II), and its typical waveform consists of the P-wave, QRS-complex, and T-wave. The QRS-complex provides distinct information in monitoring heartbeats, which can be used to discriminate the arrhythmic types. Centered on the R-wave peak, the QRS-complex can be divided into the Q-R segment and R-S segment ($P = 2$). For 50 sampling points (25 points before R-peak and 25 points after R-peak, $N = N_1 + N_2 = 50$), the remaining map parameters can be solved by Equations (7) and (8) in the Matlab workspace. By using FD between 1 and 2, the fractal patterns are constructed with Equations (5), (6), and (9). The FDTs with fractal dimension $D = 1.6$ is chosen in this study. For a QRS-complex of normal beat (Patient Number: MIT-103), related parameters c_p, d_p, f_p , and $g_p, p = 1, 2$, are computed as shown in **Table 1**. The coefficients of four terms are assigned to construct FDT functions with 4 remaining map parameters for Q-R segment and R-S segment, respectively. Following the multiplication and addition of the FDT, the fractal fractures can be computed. However, the logical blocks only support the four fundamental operations of arithmetic. In Equation (5), special function $\sin\left(\frac{\pi n'}{D}\right)$ must be expanded a function into finite terms of Maclaurin series as

$$\begin{aligned} \sin\left(\frac{\pi n'}{D}\right) &\cong \sum_{r=0}^R (-1)^r \frac{\left(\frac{\pi n'}{D}\right)^{2r+1}}{(2r+1)!} \\ &\cong \frac{\pi n'}{D} - \frac{1}{3!} \left(\frac{\pi n'}{D}\right)^3 + \frac{1}{5!} \left(\frac{\pi n'}{D}\right)^5 - \dots + \frac{1}{(2R+1)!} \left(\frac{\pi n'}{D}\right)^{2R+1} \\ &\cong z_0 (\omega n'_t) + z_1 (\omega n'_t)^3 + z_2 (\omega n'_t)^5 + \dots + z_R (\omega n'_t)^{2R+1} \end{aligned} \tag{14}$$

where $\omega = \frac{\pi}{D}$ and $n'_t = \frac{(D-1)}{(N_p - 1)}$, ω and n'_t are the

constant coefficients; $R, r = 0, 1, 2, \dots, R$, is the number of series term ($R = 10$ in this study); $z_r, r = 0, 1, 2, \dots, R$, represent the series coefficients and are also constant values. These coefficients can be computed and completed to verify the expanded function accuracy in the Matlab workspace, as shown in **Table 1**.

Figure 1 shows the structure of FDT logical block, in which 13 adders, 26 multipliers, and 17 constant coefficients are required to implement each FDT. Its CLB can design the function of feature extraction with combinational logical elements, and constant coefficients are stored in the memory elements. When each sampling data is applied to the FDT, each fractal feature is computed with multiplication and addition. This parallelism process completes the fractal pattern, and then each feature is applied to the PNN logical block.

Table 1. Related data for FDTs.

Function	The Number of FDT	Remaining Map Parameter	
W_{1x}	25	c_1	0.8811360429
		d_1	0.8485988992
		f_1	0.3445652340
		g_1	0.3857726869
W_{2x}	25	c_2	-0.6759430538
		d_2	0.9296483879
		f_2	-0.2087852761
		g_2	0.5826642888
Function	The Number of Expanded Term	Series Coefficient	
$\sin(\bullet)$	11	ω	1.9634954084
		n'_t	0.0250000000
		Z_0	1.0000000000
		Z_1	-0.1666666666
		Z_2	0.0083333333
		Z_3	-0.0001984126
		Z_4	0.0000027557
		Z_5	-2.5052108385E-8
		Z_6	1.6059043836E-10
		Z_7	-7.6471637318E-13
		Z_8	2.8114572543E-15
Z_9	-8.2206352466E-18		
Z_{10}	1.9572941063E-20		

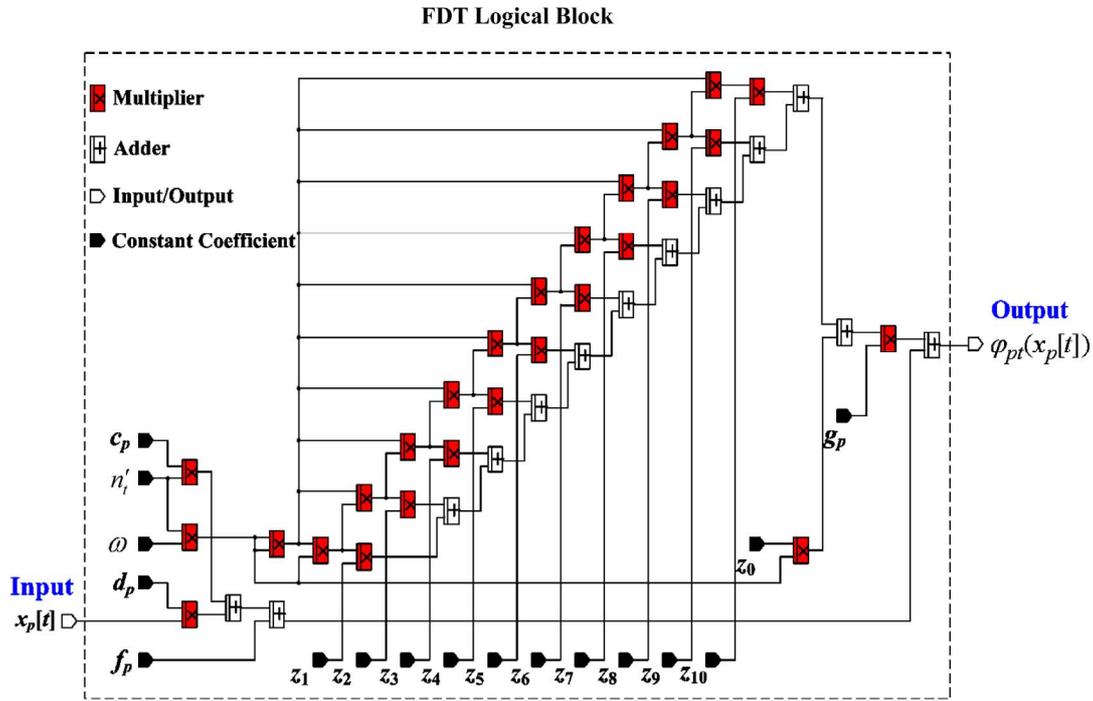


Figure 1. The structure of FDT logical block.

3.3. PNN Implementation with FPGA

In this section, we focus on classifier design and collection of the annotated ECG beats for PNN training data. The ECG signals are obtained from the MIT-BIH arrhythmia database, including patient numbers: 100, 103, 107, 109, 111, 118, 119, 124, 200, 202, 207, 209, 212, 213, 214, 217, 221, 231, 232, and 233 [21]. ECG signals have various morphological information and waveforms, which can be classified into seven categories, including normal beat (●), premature ventricular contraction (V), atrial premature beat (A), right bundle branch block beat (R), left bundle branch block beat (L), paced beat (P), and fusion of paced and normal beat (F). Centered on the R-wave peak, the QRS-complex is divided into the Q-R segment and R-S segment. The FDTs with FD are utilized to construct various fractal patterns as shown in Figure 2. With data self-similarity, the preprocess resulting in the fractal patterns are similar for the same category, which can reduce the requirement of training data. The total number of fractal patterns are selected to be 1-, 6-, 2-, 3-, 4-, 4-, and 2-set data ($K = 22$) for the seven categories, respectively. These associated patterns could be expressed as weights w_{ki}^{IH} , $k = 1, 2, 3, \dots, 22, i = 1, 2, 3, \dots, 50$, between the input and hidden layer. The weights w_{jk}^{HS} , $m = 1, 2, 3, \dots, 7$, between the hidden and summation layer are encoded as binary values with signal “1” denoting the seven categories while the rest of the weights are zero. The smoothing parameter σ was adjusted by using the gradient descent method with 22-set training

data. The optimal parameter $\sigma = 0.10942$ can be computed in the Matlab workspace. For the convergent condition ($Squared\ Error \leq 10^{-4}$), PNN converges to the nearest local minimum for less than five learning cycles. The related data of the PNN-based classifier are shown in Table 2.

3.3.1. Hidden Node CLB

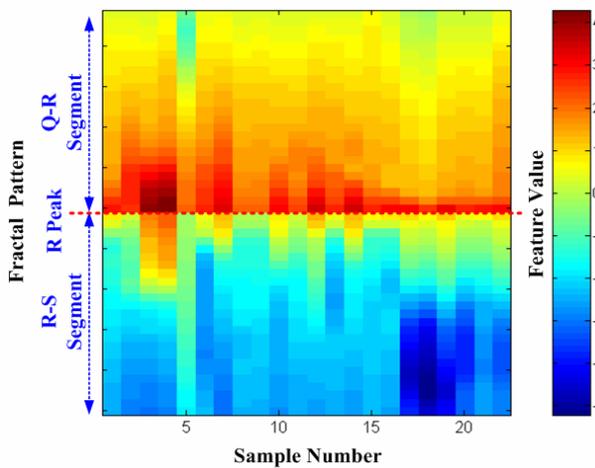
In the hidden layer, a normalized Gaussian function must be also expanded into a Maclaurin series as

$$\begin{aligned} [\exp(\delta E'_{dk})]^{-1} &\cong \left[\sum_{r=0}^R \frac{(\delta E'_{dk})^r}{(r)!} \right]^{-1} \\ &\cong \left[1 + (\delta E'_{dk}) + \frac{1}{2!}(\delta E'_{dk})^2 + \dots + \frac{1}{(R)!}(\delta E'_{dk})^R \right]^{-1} \quad (15) \\ &\cong \left[y_0 + y_1(\delta E'_{dk}) + y_2(\delta E'_{dk})^2 + \dots + y_R(\delta E'_{dk})^R \right]^{-1} \\ &= \frac{div}{\left[y_0 + y_1(\delta E'_{dk}) + y_2(\delta E'_{dk})^2 + \dots + y_R(\delta E'_{dk})^R \right]} \end{aligned}$$

where div is dividend, $div = 1$ in this study, $\delta = \frac{1}{2\sigma^2}$

and $E'_{dk} = \sum_{i=1}^N (\varphi_i - w_{ki}^{IH})^2$, δ is the constant coefficient, and

R is the number of series term ($R = 6$ in this study); y_r are the series coefficients. Related data can be computed and stored in the memory elements as shown in Table 2. The



Note: 1) No. 1: •; 2) No. 2~7: V; 3) No. 8~9: A; 4) No. 10~12: L; 5) No. 13~16: R; 6) No. 17~20: P; 7) No. 21~22: F.

Figure 2. The various fractal patterns for multiple cardiac arrhythmias.

Table 2. Related data for PNN-based classifier.

Method	Network Topology				Training Data	Learning Rate	Initial Smoothing Parameter
	I	H	S	O			
PNN	50	22	8	7	22	$0 < \eta \leq 1$	$\sigma(q=0) = 1.0$

Function	The Number of Expanded Term	Related Coefficient	
		δ	41.7615475105
		<i>div</i>	1.0000000000
		y_0	1.0000000000
		y_1	1.0000000000
exp(•)	8	y_2	0.5000000000
		y_3	0.1666666666
		y_4	0.0416666666
		y_5	0.0083333333
		y_6	0.0013888888

term $\delta E'_{dk}$ can be computed with multiplication and ad-

dition. Then input the results to Gaussian function H_k . **Figure 3** shows that the structure of hidden-node CLB, 106 adders, 63 multipliers, 1 divider, and 59 constant coefficients are required to implement each node H_k .

3.3.2. Summation-Node and Output-Node CLBs

For seven categories, the weighting factors w_{jk}^{HS} , $k = 1, 2, 3, \dots, 22, j = 1, 2, 3, \dots, 7$, are encoded as binary values with signal “1” belonging to *category j* and the rest of the factors are zero. The weighting matrix $[w_{jk}^{HS}]_{7 \times 22}$ is sparse with 22 nonzero elements. The numerator of Equation (12) is a matrix vector computation, where each output S_j is formed by multiplying each of 22 outputs of the hidden node by one of 22 weighting factors, and can be presented as

$$\begin{matrix} S_1 \\ S_2 \\ S_3 \\ S_4 \\ S_5 \\ S_6 \\ S_7 \end{matrix} = \begin{bmatrix} 1 & 0 & 0 & \dots & 0 & 0 & \dots & 0 & 0 \\ 0 & 1 & 1 & & 0 & 0 & & 0 & 0 \\ 0 & 0 & 0 & \dots & 0 & 0 & \dots & 0 & 0 \\ 0 & 0 & 0 & & 1 & 1 & & 0 & 0 \\ 0 & 0 & 0 & \dots & 0 & 0 & \dots & 0 & 0 \\ 0 & 0 & 0 & & 0 & 0 & & 0 & 0 \\ 0 & 0 & 0 & \dots & 0 & 0 & \dots & 1 & 1 \end{bmatrix} \begin{matrix} H_1 \\ H_2 \\ H_3 \\ \vdots \\ H_{11} \\ H_{12} \\ \vdots \\ H_{21} \\ H_{22} \end{matrix}$$

$$\Rightarrow \begin{matrix} \bullet \\ V \\ A \\ L \\ R \\ P \\ F \end{matrix} \begin{matrix} S_1 \\ S_2 \\ S_3 \\ S_4 \\ S_5 \\ S_6 \\ S_7 \end{matrix} = \begin{bmatrix} H_1 \\ H_2 + H_3 + H_4 + H_5 + H_6 + H_7 \\ H_8 + H_9 \\ H_{10} + H_{11} + H_{12} \\ H_{13} + H_{14} + H_{15} + H_{16} \\ H_{17} + H_{18} + H_{19} + H_{20} \\ H_{21} + H_{22} \end{bmatrix}$$

(16)

The number of addition and multiplication operations can be reduced leading to an increased speed in the arithmetic process. In the summation layer, the outputs of summation node H_k are computed with 15 adders. For the same category, their outputs of hidden nodes are summed in the summation-node CLB. The implementation of output node O_j would require 6 adders and 7 dividers, and can be presented as

$$\begin{matrix} \bullet \\ V \\ A \\ L \\ R \\ P \\ F \end{matrix} \begin{matrix} O_1 \\ O_2 \\ O_3 \\ O_4 \\ O_5 \\ O_6 \\ O_7 \end{matrix} = \begin{bmatrix} 1 \\ \frac{1}{S_1 + S_2 + S_3 + S_4 + S_5 + S_6 + S_7} \end{bmatrix} \begin{matrix} S_1 \\ S_2 \\ S_3 \\ S_4 \\ S_5 \\ S_6 \\ S_7 \end{matrix}$$

(17)

Input Layer



Figure 3. The structure of hidden-node logical block.

as shown by the denominator of Equation (12), the number of the addition operations can also be reduced. The

structure of summation-node and output-node CLBs are shown in **Figure 4**.

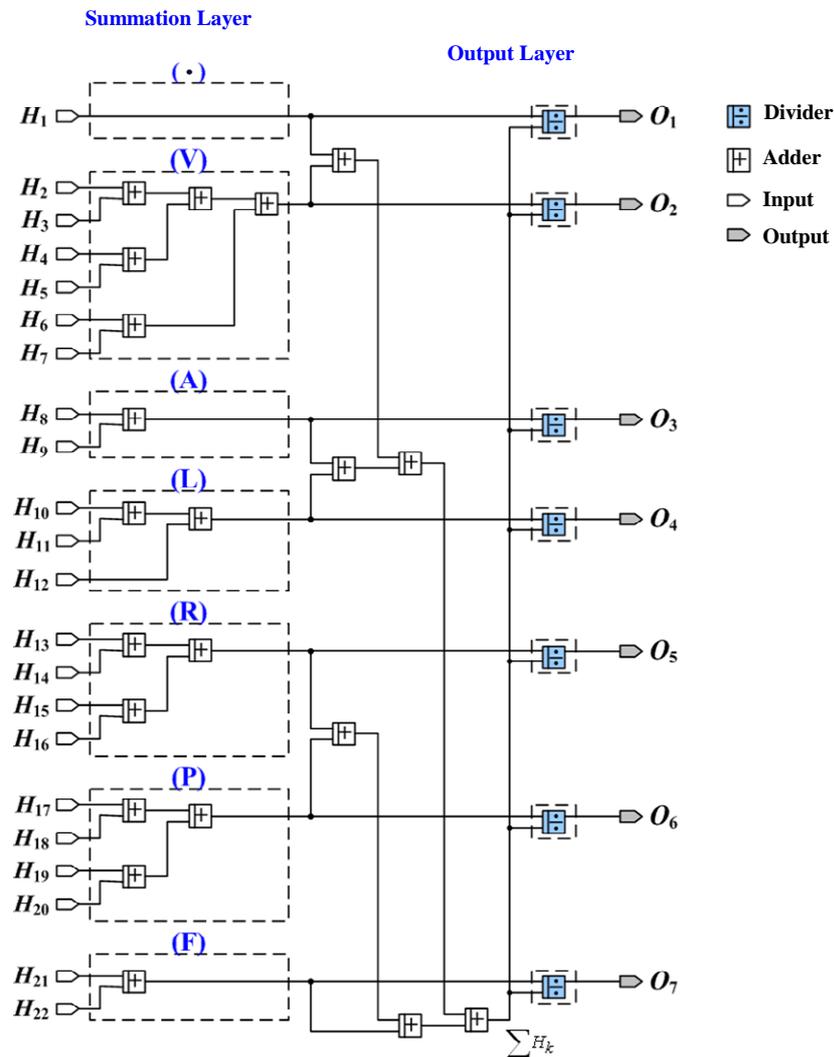


Figure 4. The structure of summation-node and output-node logical block.

3.4. Overall Structure of the Proposed Classifier

In **Figure 5**, the overall structure of the proposed classifier divides into three stages: 1) signal preprocessing; 2) fractal feature extraction; and 3) heartbeat recognition with PNN-based classifier. In the preprocessing stage, ECG signals are acquired by using the amplifier and filter. The band-pass filter is used to remove unwanted frequency components, which comprise supply line frequency interference (50 Hz/60 Hz), baseline wander, and muscle noises. Thus, these noises do not affect the performance of the proposed classifier. ECG records are composed by a modified limb lead II (ML II) sampled at 360 Hz. Then R-peak waves are detected by the Peak detection algorithm. It begins by scanning for local maxima in the absolute value of ECG data. For certain window, the search continues to look for next larger value. If this search finishes without finding a larger maximum, the current maximum is assigned as the R-peak wave. The averaging window was chosen to be

roughly the width of a typical QRS-complex. This window is at least 150 ms wide to allow for the wide QRS-complexes produced by V-heartbeats [22-24]. Centered on the detected R-peak, 25 sampling data are acquired including both Q-R segment (140 ms) and R-S segment (140 ms), respectively. In the second stage, these sampling data are converted to digital form (Signed 8-bit, 16-bit, or 32-bit Length Data) and then sent directly to the FDTs. The FDT CLBs with parallelism process are used to extract features and construct the fractal pattern. Finally, the classifier module integrates hidden-node, summation-node, and output-node CLBs for cardiac arrhythmias recognition.

4. EXPERIMENTAL RESULTS AND DISCUSSIONS

The FPGA implementation of the proposed classifier is applied to examine multiple cardiac arrhythmias. With MIT-BIH arrhythmias database, the records of patient

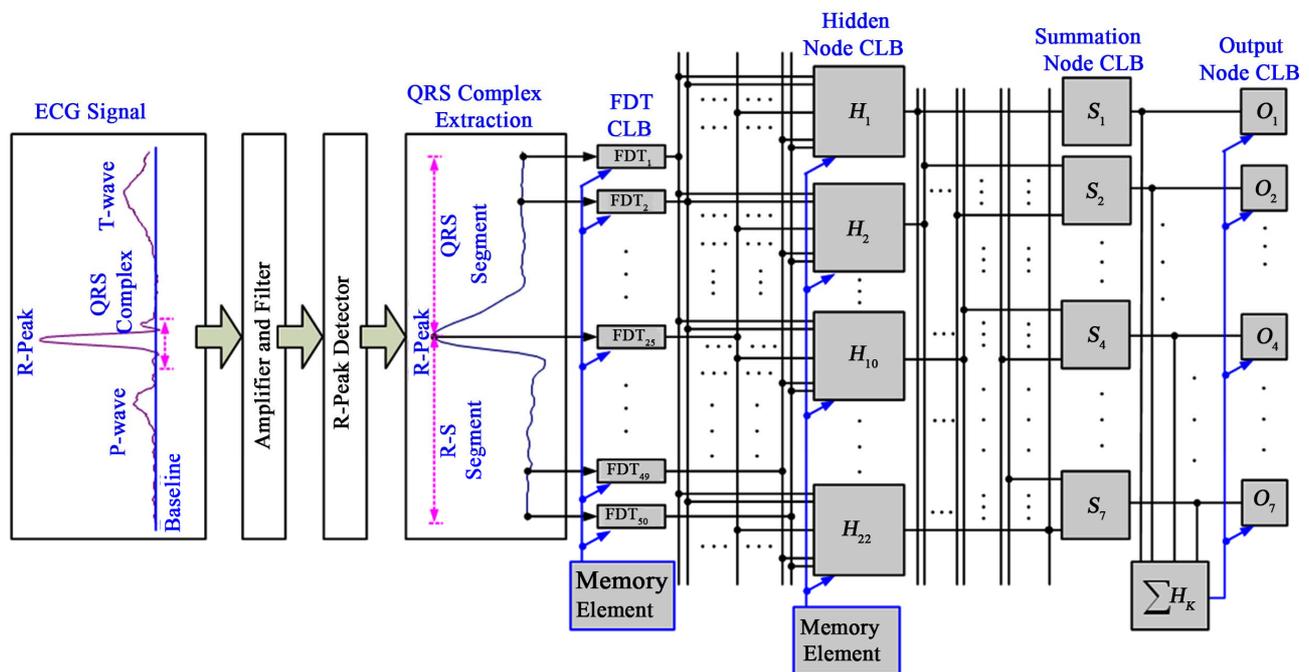


Figure 5. The overall structure of proposed fractal patterns classifier.

numbers 107, 118, 119, 200, 209, 211, 214, 217, and 231 are selected for testing. Tested ECG signals were generated using LabVIEW and Matlab software on a PC Pentium-IV, 3.0 GHz, 480 MB RAM. The design platform of SOPC-NIOS II EDA/SOPC series (NIOS II-EP2C35 Chip, 700 K system gates, EEPROM) was used in this study. The ECG signals have been digitized and band-pass filtered, thus low- and high-frequency noises appears smaller in amplitude [21]. Signal preprocesses, such as R-peak detection and QRS-complex extraction, can be performed in LabVIEW and Matlab software. It is important that the signals delivered to the FPGA must be digital type. As they are intrinsically digital formats (8-bit Format), they can be directly sent to FPGA design platform. For recorded (Training Data) and unrecorded data, the proposed classifier was tested with accuracy and computational efficiency, and compares with the results in FPGA module and Matlab workspace.

4.1. Comparison with the Fractal Patterns in FDT CLB and in Matlab Workspace

The proposed classifier is tested with the software simulation, in order to examine the implementation of FPGA modules. After the designated modules, the designated circuit can be programmed into the FPGA chip through the download cable. In feature extraction, fractal features are extracted by using 50 FDTs. Then 50 features are reconstructed into one fractal pattern. Since the FDT module is a simplified module, it is worth noting that each FDT function must be first examined before programming

them into the FPGA chip. The average fractal patterns from the same category are obtained from the selected patients. For training data, fractal patterns are computed by FDT module and high-level programming language (HLPL) in the Matlab workspace, respectively. **Figure 6** shows the comparison fractal patterns in FDT module and Matlab workspace. The asterisk-line stands for the computed data with HLPL, and plus-sign-line is the computed data with FDT module. Through cursory observation, nice insculations can be seen between them, such as the fractal patterns of normal heartbeat, V-heartbeat, and F-heartbeat (Patient Numbers: 100, 107, 119, and 200). The differences are less than 0.2 as shown by the circle-line in **Figure 6**. This confirms that the proposed FDT module has high confidence of computation performance for reconstructing fractal patterns.

4.2. Classification Tests

The learning performance of the proposed classifier was tested with 22-set training data. In the learning stage, the optimal parameter σ can be computed in the Matlab workspace. The proposed method has a fast learning process with slight iteration for adjusting parameter σ . It takes 0.195 seconds to classify the 22-set training data into 7 categories. Then this optimal value was used to determine the parameter σ of 22 hidden-node modules and was obtain to minimize the misclassification errors. Under the optimal parameter, decision boundaries can become increasingly non-linear, the network approaches a nearest neighboring classifier. In the recalling stage, all outputs

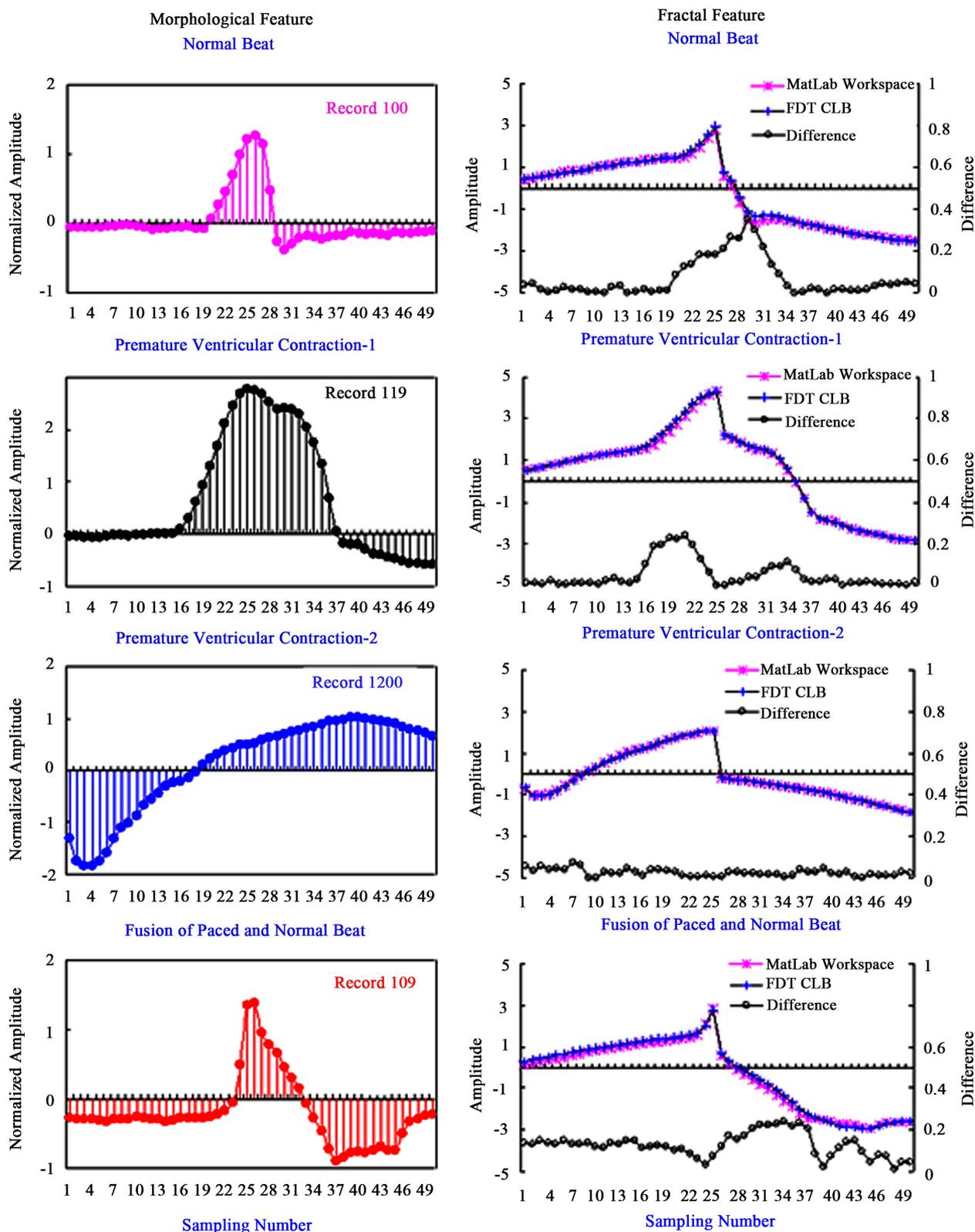
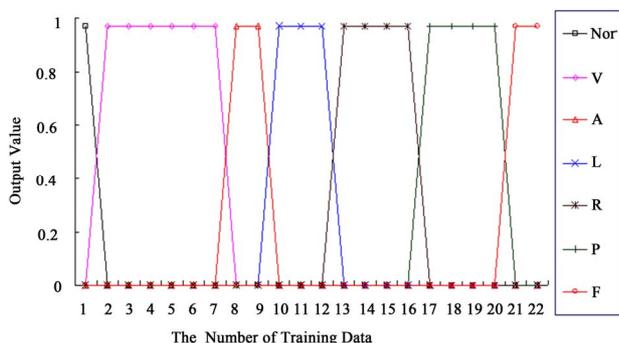


Figure 6. Compare with the fractal patterns in FDT module and in Matlab workspace.

approach the desired targets for 7 categories. The output values of the proposed classifier are shown in **Figure 7**.

This confirms that the proposed classifier has nice learning performance.



Note: 1) No. 1: ●; 2) No. 2-7: V; 3) No. 8-9: A; 4) No. 10-12: L; 5) No. 13-16: R; 6) No. 17-20: P; 7) No. 21-22: F.

Figure 7. Output target value of the proposed classifier.

Clinical diagnostic subjects have multiple cardiac arrhythmias such as supraventricular ectopic beat, ventricular ectopic beat, bundle branch ectopic beat, fusion, and paced beats. For example, patient number 200 has normal heartbeats and V-heartbeats with annotation labels in 1.5 minute segment. Test results reveal that the accuracy is 94% as shown in **Table 3**. The processes recognized 38 V-heartbeats with 6 failures, and the expected sensitivity as the fraction of category V correctly classified is 84.2%, and the specificity for normal heartbeats is 100%. The results confirm that the major category is the premature ventricular contraction. Patient number 217 has V-heartbeats, P-heartbeats, and fusion heartbeats (F). As shown in **Table 3**, test results confirm that the major category is P. The processes recognized 94 P-heartbeats with 5 failures, the sensitivities for ectopic beats is 94.7%, and the accuracy is 95%. Through the experimental tests, the proposed classifier can also recognize multiple cardiac arrhythmias with good accuracy in the FPGA module.

4.3. Discussion

In this study, the parameters of FDT functions have been directly computed by Collage theorem. Each FDT CLB has the same structure; it only assigns the segmented remaining map parameters and series coefficients. Most of them are repeatable uses. Owing to the enhancement in features by the FDT functions, the number of training data, data storage, and processing needs can be reduced. For classification applications, artificial neural network (ANN) has been presented for this study. However, it has some limitations including very slow learning process, need iteration for updating weights, and need to determine the network architecture such as the number of hidden layers and hidden nodes. The weights, input-layer to hidden-layer and hidden-layer to output-layer, are always non-zero values. This will increase the requirement of the addition and multiplication operations and memory storage. In addition, sigmoid activation functions of hidden and output nodes [25] are difficult to implement the CLB mod-

Table 3. The results of multiple cardiac arrhythmias.

Record	Method	Number of Arrhythmias						Accuracy (%)	
		●	V	A	L	R	P		F
107	Actual	0	0	0	0	0	100	0	-
	Test 1	0	3	0	0	0	96	1	96%
	Test 2	0	3	0	0	0	96	1	96%
118	Actual	0	1	0	0	99	0	0	-
	Test 1	0	2	0	0	98	0	0	99%
	Test 2	0	2	0	2	98	0	0	99%
119	Actual	75	25	0	0	0	0	0	-
	Test 1	75	25	0	0	0	0	0	100%
	Test 2	75	25	0	0	0	0	0	100%
200	Actual	62	38	0	0	0	0	0	-
	Test 1	62	32	0	0	6	0	0	94%
	Test 2	62	32	0	0	6	0	0	94%
209	Actual	99	0	1	0	0	0	0	-
	Test 1	99	0	1	0	0	0	0	100%
	Test 2	99	0	1	0	0	0	0	100%
211	Actual	0	0	0	100	0	0	0	-
	Test 1	0	0	3	97	0	0	0	97%
	Test 2	0	0	3	97	0	0	0	97%
214	Actual	0	5	0	95	0	0	0	-
	Test 1	1	4	1	92	2	0	0	96%
	Test 2	1	4	1	92	2	0	0	96%
217	Actual	0	3	0	0	0	94	3	-
	Test 1	0	3	0	2	0	89	6	95%
	Test 2	0	3	0	2	0	89	6	95%
231	Actual	0	0	0	0	100	0	0	-
	Test 1	3	0	0	0	97	0	0	97%
	Test 2	3	0	0	0	97	0	0	97%

Note: 1) Accuracy(%) = (N_c/N_t) × 100%, the overall accuracy is the fraction of the total heartbeats correctly classified; N_c: the number of correctly discriminated beats; N_t: total number of heartbeats; 2) Test 1 is the result in the Matlab workspace; 3) Test 2 is the result in FPGA module.

ules, including the arithmetic process and memory storage. The proposed classifier provides a promising way for implementing the portable bio-monitor and telemedicine.

5. CONCLUSION

A fractal-pattern classifier using FPGA for the realization of FDTs and PNN to recognize multiple cardiac ar-

rhythmias was proposed. The FDT modules are employed to construct various fractal patterns, and make the difference between normal and unhealthy subjects. The PNN module is proposed for recognizing multiple cardiac arrhythmias. Numerical experiments have been conducted with MIT-BIH arrhythmia database. The proposed classifier has excellent computational efficiency, high accuracy, and flexibility for patterns recognition. Then programs were downloaded to the FPGA chip to integrate all the modules, real-time processing, compression, transmission and input/output. This prototype can be further integrated in telemedicine and portable non-invasive devices.

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