Thermal analysis of different tips for various operating modes of phacoemulsification system

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ABSTRACT

Cataract is an opacity that develops in the crystalline lens of the eye, due to alteration in some of its protein fibers, with the consequent impairment of visual acuity. The most effective and common treatment is to surgically remove the cloudy lens. In this process the crystalline lens are removed and the eye's refraction power is restored by inserting an artificial lens. Phacoemulsification refers to modern cataract surgery in which the eye's internal lens is emulsified with an ultrasonic hand piece, and aspirated from the eye. Aspirated fluids are replaced with irrigation of balanced salt solution, thus maintaining the anterior chamber, as well as cooling the hand piece. The patient can be released soon after the operation. The problem of this procedure in some cases is thermal damage. This research addresses the aforementioned problem through an important parameter, different operating modes of the system. The proposed in-vitro approach has been investigated in details.

Keywords: Cataract Surgery; Phacoemulsification; Thermal Damages; In Vitro Measurement; Thermocouples

1. INTRODUCTION

When the natural lens of eye becomes cloudy, usually because of the aging process, it keeps light rays from passing through or diffuses the light in such a way that vision becomes fuzzy or hazy. This cloudy lens is called a cataract. The object of cataract surgery is to remove this hazy lens and to replace it with a plastic prescription lens that is permanently implanted in the eye.

At present, the most widely used surgical technique is phacoemulsification, developed by Kelman (1967), in which ultrasonic emissions are utilized to fragment the crystalline lens inside the eye, the fragments then being drawn out through a very small incision – about 2.8-3 mm – at the zone where the cornea meets the sclera. This technique has several advantages such as faster surgical times, smaller incisions which make healing times quicker and increased surgeon control [2,3].

Three components constitute the heart of all phaco systems which are irrigation, aspiration and ultrasound [4].

The ultrasonic hand piece (Figure 1) incorporates a transducer for converting high-frequency, alternating current in to mechanical vibrations. By piezoelectric crystals electrical energy converts to mechanical energy and causes the hollow cylindrical tip attached to oscillate at frequency around 40 KHz to break up (emulsify) the cataract into tiny pieces [1,2].

The emulsified material is simultaneously suctioned from the eye by the tip. The front (anterior) section of the lens capsule is removed along with the fragments of the natural lens. The back (posterior) portion of the capsule is left in place to hold and maintain the correct position for the implanted intraocular lenses.

2. DISCUSSION

2.1. Lead-In

With an increase in the use of phacoemulsification concern about potential for thermal wound injuries during surgery has increased [9]. Phacoemulsification requires more attention to detail than any other ophthalmic surgical procedure. The success of each step of the procedure is critically dependent upon how well each previous



Figure 1. Phacoemusification hand piece.



step was performed. Errors early in the procedure will almost inevitably result in subsequent problems.

The small incision is what gives phaco most its advantages but, as with all steps in phacoemulsification, it must be fashioned very exactly [5].

The location, the size, the depth and configuration of the incision are all very critical factors in determining the final outcome in phaco.

In some cases burns can result in fusion of the cornea or the sclera, damage the corneal endothelium, wound gape and delayed wound healing.

It is important to note that the aim of this study is to compare and analyze the changes of temperature around the different tips for three operating modes of Sina Phacoemulsification System (**Figure 2**) which is one of the products of an Iranian medical engineering company (Aali-Payam Corporation) [9,10].

2.2. Instruments and Methodology

In this study, for the purpose of monitoring in vitro the changes of temperature values are based on the utilization of two different types of thermocouples;

- 1) Digital Thermocouple
- 2) Thin wires Thermocouple

In all of experimental tests the tip is in the chamber with dimension of 10 cm \times 18 cm \times 23 cm which is full of serum solution (Sodium Chloride 0.9%). The size of chamber is big enough so it acts as a thermal bath. Power of system is on its pre-set value, 50% and intensity of waves for this power are about 155 W/cm² [10,11].

2.2.1. Digital Thermocouple

Digital thermocouple has a probe and can measure temperatures near the phaco tip with sensitivity of 0.01° C. In measurement with digital thermocouple, each experimental test is repeated 5 times for every mode and the averages of temperature changes in a period of 60 seconds are plotted.

2.2.2. Thin Wires Thermocouple

Thin wires thermocouple which is made of two different metal wires (Ni-NiCr) with sealing wax on them for prevention of RF (radio frequency) waves [6]. With four thin wires thermocouple temperatures are measured in four different areas (**Figure 3**) near the tip indirectly by the changes of voltage with sensitivity of 1 μ V and simultaneously are drawn by an X-Y recorder.

On the next stage temperature changes are measured by thin wires thermocouple for the same tip in a period of 60 seconds with the same initial conditions.

Because voltage changes are in the order of μV , then the numbers of peaks in a specific period of time are greater so in these graphs four points are important for us in comparison; starting point, maximum, minimum



Figure 2. Sina phacoemulsification system (Aali-Payam Co.).



Figure 3. Four different thin wires thermocouples monitor the temperature changes of the tip.

and ending.

According to the position of operator's foot on the pedal of system, four positions are defined [7].

Position 0: Foot is off the pedal, no action.

Position 1: Initial depression of foot pedal. Fluid flows from the bottle, no aspiration or emulsification.

Position 2: Pedal pushed to the detent. Aspiration now accompanies irrigation.

Position 3: Pedal pressed to the next detent. With phaco hand piece, emulsification now is added to irrigation and aspiration.

Three operating modes were analyzed;

1) Linear mode, in this mode the power of ultrasound waves are increased gradually from zero to the preset power of the system and it directly depends on how far down the pedal is pushed

2) Constant mode, in this mode the power of ultrasound emissions are equal to the preset power of system immediately in the stages in which waves were used

3) Pulse mode, in this mode the ultrasonic stream is not continuous but pulsed [8]

Phacoemulsifier tips come in a number of variations;

728

the three common ones are named for the angle of the cutting area. They are 0 degree, the 15 degree, the 30 degree and the 45 degree.

The 45 degree tip has the longest bevel and therefore the sharpest tip, so it cuts most easily. Because of the large bevel of the aspiration port it occludes less easily.

The 30 degree tip has smaller bevel. Therefore the port is smaller and occludes more easily so it is more efficient for the aspiration.

Some surgeons like to vary the tip depending on the density of the cataract: using a 45 degree tip for a hard cataract and a 30 degree tip for softer cataracts and they are the most popular so we have done all of the measurements and comparisons for these two tips.

3. ANALYSIS OF RESULTS

In this study, for the purpose of monitoring in vitro the temperature values around two tips with the angle of 30 and 45 degree, first the measurements are done by digital thermocouple for different operating modes of phaco system. On the next stage, same measurements are done but with thin wires thermocouples.

3.1. 30 Degree Tip – Digital Thermocouple

Shown in **Figure 4** and **Table 1** are the temperature values monitored by digital thermocouple during system is operating in linear and constant modes for the 30 Degree tip. In linear mode maximum temperature increase is 0.5 °C but in constant mode it is 0.47°C.

Shown in **Figure 5** and **Table 2**, in pulse mode, when the system is set to emit 10 pulses per second (pps), maximum temperature increase for linear – pulse mode around the tip is 0.2° but for constant – pulse mode this value is 0.23° C.

3.2. 30 Degree Tip – Thin Wires Thermocouples

In **Table 3**, the temperature values reached in linear and constant modes around the tip which are measured by thin wires thermocouples in four different areas around the 30 Degree tip is shown.

Figure 6 are the temperature changes that are plotted according to the voltage changes of each thermocouple versus time in linear mode.

The maximum temperature increase in this mode for thermocouples No.1 is 48, No.2 is 15, No.3 is 112 and No.4 is 69μ V.

Figure 7 are the temperature changes that are plotted according to the voltage changes of each thermocouple versus time in constant mode.

The maximum increase in this mode for thermocouples No.1 is 56, No.2 is 19, No.3 is 97 and No.4 is 83 μ V.

In Table 4, the temperature values reached in linear –

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Figure 4. Linear mode – temperature values versus time [left]; constant mode – temperature values versus time [right].

 Table 1. Temperature values for linear and constant modes

 measured by digital thermocouple.

	Average of Starting	Average of Maximums	Average of Minimums	Average of Endings
LINEAR MODE	21.62	22.12	21.87	22.1
CONSTANT MODE	21.65	22.12	21.87	22.12

Table 2. Temperature values for linear – pulse and constant – pulse modes measured by digital thermocouple.

	Average of Starting	Average of Maximums	Average of Minimums	Average of Endings
LINEAR Pulse mode	22.05	22.25	22.1	22.27
CONSTANT PULSE MODE	21.62	21.85	21.72	21.82

pulse and constant – pulse modes around the tip which are measured by thin wires thermocouples in four different areas around the tip is shown.

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Figure 5. Linear-pulse mode (10 pps) – temperature values versus time [left]; constant-pulse mode (10 pps) - temperature values versus time [right].

Table 3. Temperature values for linear and constant modes measured by thin wire thermocouples.

		Starting	Maximum	Minimum	Ending
LINEAR MODE	THERMO NO.1	-10	38	8	22
	THERMO NO.2	-3	12	-1	-2
	THERMO NO.3	-10	102	35	80
	Thermo No.4	-4	65	41	50
	Thermo No.1	-2	54	12	31
Con- stant mode	THERMO NO.2	-2	17	1	2
	THERMO NO.3	3	100	59	89
	THERMO NO.4	1	84	21	67





Figure 6. Linear mode – voltage changes (μV) versus time (sec.) for each thermocouple.



Figure 7. Constant mode – voltage changes (μ V) versus time (sec.) for each thermocouple

Table 4. Temperature values for linear – pulse and constant – pulse modes measured by thin wire thermocouples.

		Starting	Maximum	Minimum	Ending
	THERMO NO.1	2	31	18	27
LINEAR	THERMO NO.2	-8	8	1	2
Pulse mode	THERMO NO.3	-3	57	38	37
	Thermo No.4	-5	61	53	52
Constant Pulse Mode	THERMO NO.1	-11	21	8	10
	THERMO NO.2	-2	17	9	11
	THERMO NO.3	12	63	48	57
	THERMO NO.4	6	90	78	9

Figure 8 are the temperature changes that are plotted according to the voltage changes of each thermocouple versus time in linear – pulse mode when the system is set to emit 10 pulses per second (10 pps). The maximum increase in this mode for thermocouples No.1 is 29, No.2 is 16, No.3 is 60 and No.4 is 66 μ V.

Figure 9 are the temperature changes that are plotted according to the voltage changes of each thermocouple versus time in constant – pulse mode when again the system is set to emit 10 pulses per second (10 pps).

The maximum increase in this mode for thermocouples No.1 is 32, No.2 is 19, No.3 is 51 and No.4 is 84 μ V.

3.3. 45 Degree Tip – Digital Thermocouple

Shown in **Figure 10** and **Table 5** are the temperature value monitored by digital thermocouple during the system is operating in linear and constant modes for the 45 Degree tip.

In linear mode maximum increase is 0.72°C but in



Figure 8. Linear – pulse mode (10 pps) – voltage changes (μ V) versus time (sec.) for each thermocouple.



Figure 9. Constant – pulse mode (10 pps) – voltage changes (μV) versus time (sec.) for each thermocouple.

constant mode it is 0.67℃.

Shown in Figure 11 and Table 6, in pulse mode, when the system is set to emit 10 pulses per second (10 pps), maximum increase for linear – pulse mode around the tip is 0.17° C but for constant – pulse mode this value is 0.13° C.

3.4. 45 Degree Tip – Thin Wires Thermocouples

In **Table 7**, the temperature values reached in linear and constant modes around the tip which are measured by thin wires thermocouples in four different areas around the tip is shown.

Figure 12 are the temperature changes that are plotted according to the voltage changes of each thermocouple





Figure 10. Linear mode – temperature values versus time [left]; constant mode – temperature values versus time [right].

 Table 5. Temperature values for linear and constant modes

 measured by digital thermocouple.

	Average of Starting	Average of Maximums	Average of Minimums	Average of Endings
LINEAR MODE	20.35	21.07	20.92	20.97
CONSTANT MODE	20.35	21.02	20.85	21.12



Figure 11. Linear -pulse mode (10 pps) – temperature values versus time [left]; constant -pulse mode (10pps) – temperature values versus time [right].

 Table 6. Temperature values for linear – pulse and constant –

 pulse modes measured by digital thermocouple.

	Average of Starting	Average of Maximums	Average of Minimums	Average of Endings
LINEAR PULSE MODE	21.40	21.57	22.55	21.62
CONSTANT PULSE MODE	20.57	20.70	20.65	20.72

versus time in linear mode.

The maximum increase in this mode for thermocouples No.1 is 40, No.2 is 32, No.3 is 47 and No.4 is 13 μ V.

Figure 13 are the temperature changes that are plotted according to the voltage changes of each thermocouple versus time in constant mode.

The maximum increase in this mode for thermocouples No.1 is 9, No.2 is 19, No.3 is 64 and No.4 is 67 μ V.

In **Table 8**, the temperature values reached in linear – pulse and constant – pulse modes around the tip which are measured by thin wires thermocouples in four different areas around the tip is shown.

 Table 7. Temperature values for linear and constant modes measured by thin wire thermocouples.

		Starting	Maximum	Minimum	Ending
LINFAR	THERMO NO.1	0	40	-2	9
	THERMO NO.2	-9	23	7	18
MODE	THERMO NO.3	-7	40	0	8
	Thermo No.4	-7	6	0	2
Constant Mode	Thermo No.1	-5	4	-10	2
	THERMO NO.2	-8	11	-2	2
	THERMO NO.3	-14	50	10	15
	THERMO NO.4	-5	62	32	56
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Thermocouple No.3

Thermocouple No.4

Figure 12. Linear mode – voltage changes (μV) versus time (sec.) for each thermocouple.



Figure 13. Constant mode – voltage changes (μV) versus time (sec.) for each thermocouple.

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		Starting	Maximum	Minimum	Ending
	THERMO NO.1	0	12	-4	6
LINEAR	THERMO NO.2	0	26	16	23
Pulse mode	THERMO NO.3	-2	12	-1	0
	THERMO NO.4	4	58	33	54
Constant Pulse Mode	THERMO NO.1	-12	4	-8	2
	THERMO NO.2	6	30	8	21
	THERMO NO.3	-5	18	-7	-3
	THERMO NO.4	9	40	16	33

 Table 8. Temperature values for linear – pulse and constant –

 pulse modes measured by thin wire thermocouples.

Figure 14 are the temperature changes that are plotted according to the voltage changes of each thermocouple versus time in linear – pulse mode when the system is set to emit 10 pulses per second (10 pps). The maximum increase in this mode for thermocouples No.1 is 12, No.2 is 26, No.3 is 14 and No.4 is 54 μ V.

Figure 15 are the temperature changes that are plotted according to the voltage changes of each thermocouple versus time in constant – pulse mode when the system is set to emit 10 pulses per second (10 pps).

The maximum increase in this mode for thermocouples No.1 is 16, No.2 is 24, No.3 is 23 and No.4 is 31 μ V.

4. CONCLUSION

In this study thermocouples have been used as an instrument for measuring the temperature changes of different tips to monitor and compare three operating mode of phacoemulsification system.

All in vitro measurements are done with the same initial conditions. In evaluating the maximum temperature reach in each operating mode, it has been found that for both tips temperature changes in pulse mode (linear – pulse and constant – pulse) has fewer and lower peaks. The main reason is the periods of short time between each pulsed wave allow the tip to get cool between two successive emissions. Moreover, in these modes, the system produces a lower thermal increase with respect to the linear and constant modes.

It is strongly recommend that in cataract surgery with Sina phaco system only linear – pulse and constant –



Figure 14. Linear – pulse mode (10 pps) – voltage changes (μV) versus time (sec.) for each thermocouple.



Figure 15. Constant – pulse mode (10 pps) – voltage changes (μV) versus Time (sec.) for each thermocouple.

pulse modes should be used, so to reduce any possible surgical complications caused by the excessive release of heat.

At the end it should be mentioned that although all the experimental tests were performed in vitro and thermal increasing of tip during surgical operation is higher than these data, the results suggest this modern procedure can be performed at a safe temperature with the knowledge-able selection of surgeon-controlled parameters.

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