

# Preparation of Biocompatible Magnetic Microspheres with Chitosan

Mohamed K. Nasra, Moustafa M. Mohamed, Mohamed A. Elblbesy, Bothaina A. Hefney

Medical Biophysics Departement, Medical Research Institute, Alexandria University, Alexandria, Egypt.  
Email: M.Abdulaziz.Elblbesy@gmail.com

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## ABSTRACT

*Microsphere is a term used for small spherical particles, with diameters in the micrometer range (typically 1  $\mu\text{m}$  to 1000  $\mu\text{m}$  (1 mm)). Microspheres are sometimes referred to as microparticles. Microspheres can be manufactured from various natural and synthetic materials. The present work we prepared chitosan magnetic microspheres (CMMS) with simple crosslinking method. The obtained CMMS were in size range of 1000 - 2600 nm with average particle size of 1800 nm. All the essential characterizations of prepared CMMS were done and the results were in a good agreement with other magnetic microspheres prepared with different method. To test the biocompatibility of CMMS with blood, the effect of them on erythrocytes aggregation and blood hemolysis were studied. Our results showed that CMMS work as good compatible materials with blood.*

**Keywords:** *Magnetic, Microspheres, Chitosan*

## 1. Introduction

Monodispersed nano/micrometer scale magnetic particles have drawn considerable attention because of both fundamental physics involved and technical applications in high-density magnetic storage media, ferrofluids and catalysts. The nano/micrometer spinel ferrite particles have great potential applications since they are relatively inert and their magnetic properties can be finely tuned by chemical manipulations. Especially, in recent years, the interests in monodispersed spinel ferrite nano/micrometer particles are growing based on their potential applications in biomedicine and biotechnology for contrast enhancement of magnetic resonance imaging (MRI) and as drug carriers for magnetically guided site-specific drug delivery [1].

Magnetic nanoparticles offer some attractive possibilities in biomedicine. First, they have controllable sizes ranging from a few nanometers, which places them at dimensions that are smaller than or comparable to those of a cell (10 - 100  $\mu\text{m}$ ), a virus (20 - 450 nm), a protein (5 - 50 nm) or a gene (2 nm wide and 10 - 100 nm long). This means that can 'get close' to a biological entity of interest. Indeed, they can be coated with biological molecules to make them interact with or bind to a biological entity, thereby providing a controllable means of "tag-

ging" or addressing it. Second, the nanoparticles are magnetic, which means that they obey Coulomb's law, and can be manipulated by an external magnetic field gradient. This 'action at a distance', combined with the intrinsic penetrability of magnetic fields into human tissue, opens up many applications involving the transport and/or immobilization of magnetic nanoparticles, or of magnetically tagged biological entities. In this way they can be made to deliver a package, such as an anticancer drug, or a coherent of radionuclide atoms, to a targeted region of the body, such as a tumor. Third, the magnetic nanoparticles can be made to resonantly respond to a time-varying magnetic field, with advantageous results related to the transfer of energy from the exciting field to the nanoparticles [2].

In recent years, a large number of different clinical applications of magnetic microspheres have been proposed, mainly connected to disease treatments. On the contrary, only few others have proposed to use nanoparticles for the reliable detection and localization of tumors. Magnetic drug delivery by particulate carriers is a very efficient method of delivering a drug to a localized disease site. In magnetic targeting, a drug or therapeutic radioisotope is bound to a magnetic compound, injected into a patient's blood stream, and then stopped with a powerful magnetic field in the targeted area [3].

There is a considerable interest in preparation of magnetite ( $\text{Fe}_3\text{O}_4$ ) due to its strong magnetic properties, which were used first in biology and then in medicine for the magnetic separation of biochemical products and cells as well as the magnetic guidance of particle systems for site-specific drug delivery. However, the size, charge, and surface chemistry of magnetic particles could strongly influence their magnetic properties and distribution in biological systems. The most common method for the synthesis of magnetite is by co-precipitation from a solution of Fe (III) and Fe (II) salts in presence of base. Preparation of size-controllable magnetite nano-particles was performed in presence of different water-soluble polymers such as lignosulfonate, mesoporous sulfonated styrene-divinylbenzene, polypeptide [4,5] etc.

Magnetite nano-particles have been also incorporated into more complicated architectures, such as polymeric gels providing formation of magnetic field sensitive gels [6]. These gels contain magnetic particles dispersed homogeneously and confined in a polymer network. Under a nonuniform magnetic field, the particles undergo motion; which in turn induces elongation, contraction, or bending of the gels with short response time. Incorporation of magnetite into spherical polymeric particles has been achieved by following two approaches: 1) heterocoagulation of magnetite on the surface of pre-formed polymeric particles [7], 2) encapsulation of magnetite particles during emulsion polymerization process [8] or by using the microemulsion approach [9], or 3) by layer-by-layer deposition method [10,11].

As the pharmaceutical industry continues to develop new effective medications, the need to develop efficient, minimally invasive delivery techniques is paramount. A successful targeted drug delivery system will allow clinical usage of drug not currently accessible to physicians, as well as a more efficient means for delivering those already available [12].

Chitosan is a heteropolysaccharide composed of  $\beta$ -(1-4)-2-deoxy-2-amino-d-glucopyranose units and of  $\beta$ -(1-4)-2-deoxy-2-acetamino-d-glucopyranose units. Chitosan occurs in nature, particularly in the cell wall of some fungi such as *Mucor rouxii* [13] and is mainly produced by the deacetylation of chitin, which is a major component of the exoskeleton of insects, the cuticles of annelids and mollusks, and the shell of crustaceans such as shrimp, crab, and lobster. Chitosan has been extensively examined in the pharmaceutical industry for its potential in the development of controlled release of drug delivery due to its excellent biocompatibility, biodegradability, bioactivity and nontoxicity [14]. Various sustained release drug carriers have been made from chitosan such as microparticles [15], tablets [16], gel [17] and beads [18]. Chitosan microspheres have been widely investigated for use as controlled release delivery sys-

tems for hormones [19], vitamins [20], proteins [21] and enzymes [22].

This work aims to prepare the chitosan magnetic microspheres and to study its effect on dynamic properties (blood viscosity, erythrocytes aggregation, osmotic fragility and hemolysis) (*in vitro*) under the influence on external magnetic field.

## 2. Materials and Methods

Chitosan polymer, glutaraldehyde, Sodium hydroxide, ferrous sulfate, ferric chloride, sodium hydroxide and polyethylene glycol-10000 (PEG-10000) were obtained from Sigma (UAS). All chemicals were of analytical grade and no further purification was required.

### Preparation of Chitosan Magnetic Microspheres

Acetate buffer was used as solvent for the chitosan polymer and glutaraldehyde was used as the cross-linker. Sodium hydroxide solution was used as medium. Magnetic fluid was synthesized as follows: a 35% (w/v) ferrous sulfate solution, 54% (w/v) ferric chloride solution and 36% (w/v) sodium hydroxide solution were prepared using distilled water. Then the ferric salt and ferrous salt were mixed, stirred and heated. When the temperature reached 55°C, the alkaline solution was added. The mixture was stirred for 30 min, and then 5 g of polyethylene glycol-10000 (PEG-10000) was added. The temperature was raised to 80°C and maintained for 30 min. The mixture was then neutralized while cooling, and the magnetic fluid was prepared. 1% (w/w) chitosan was dissolved in acetate buffer at pH 4.5. The dissolved chitosan was added drop wise on the magnetic fluid using Syringe Pump. Formed CMMS were washed with deionized water and soaked in 1, 3, and 5 mol % glutaraldehyde solution for 2 hr, and then washed with deionized water.

Scanning electron microscopy (SEM) (Joel, JSM-6360 LA-Japan) images were taken after sputter coating the CMMS with gold (SPI-module TM Sputter coater, Japan). the size of CMMS was analyzed by Beckman Coulter Particle Size Analyzer (N5 submicron particle size analyzer, Japan). The magnetic properties of air dried MMS were determined by a vibrating-sample magnetometer (VSM-9600-1DSM-LDG-USA). Thermo gravimetric analyses (TGA) were measured by (Shimadzu, TGA-50, Japan) with a heating rate of 10°C/min in nitrogen flow. Fourier transforms infrared spectrophotometer (FT-IR) spectra were recorded before and after processing of CMMS. The FTIR spectra were obtained using a FT-IR spectrophotometer (Alpha-centauri) (Shimadzu, Japan, FT-IR-8400S). Around 4 - 8 mg of MMS were thoroughly mixed with IR-grade potassium bromide (KBr) (200 mg) and grinding together, then compressed into tablet form with the compressor (Shimadzu-Compressor-Japan) in order to record the spectrum.

### Microscopic Study of RBC's Aggregation

For examine the effect of CMMS on erythrocytes aggregation. 2 ml of erythrocytes suspension with 1% concentration in PBS was incubated with 1 gm of CMMS for two hours. The incubated erythrocytes were then allowed to immigrate freely on an inclined slide at angle of 45° in order to make erythrocytes film [23]. Erythrocytes film was left to dry for two minutes. The erythrocytes film was examined using light microscope connected to CCD camera. The image of erythrocytes film was transferred to computer through an interface connected to CCD camera. The images of erythrocytes film were analyzed by imaging processing software in order to calculate aggregation shape parameter (ASP) which is used to quantify erythrocytes aggregation. The following equation was used to calculate ASP [24]:

$$ASP = 4\pi A/P^2 \quad (1)$$

where A is the projected area of the aggregate, P is the perimeter of the projected area. The ASP of ten images of incubated erythrocytes was computed in order to calculate the mean value of ASP and then compared to the mean value of unincubated erythrocytes.

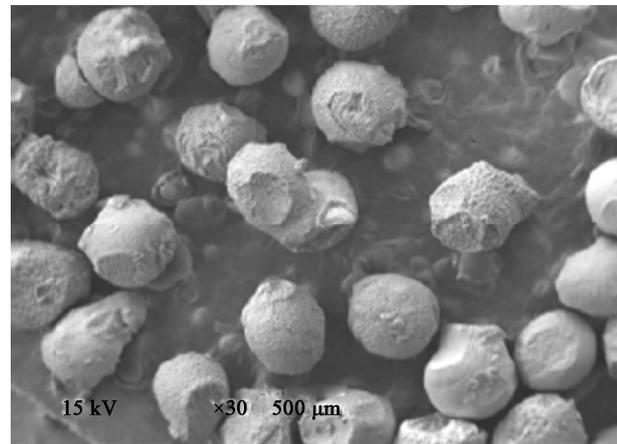
### Hemolysis

Hemolysis has been determined to confirm that the chosen magnetic field intensity for the chosen time period affects the cellular membrane. Erythrocyte suspensions (Ht = 5%) was incubated with CMMS, for two hours. After centrifugation the degree of hemolysis (%) was determined by measuring the hemoglobin content in the supernatant at 540 nm. Hemolysis was expressed as a percentage of the absorbance in distilled water [25].

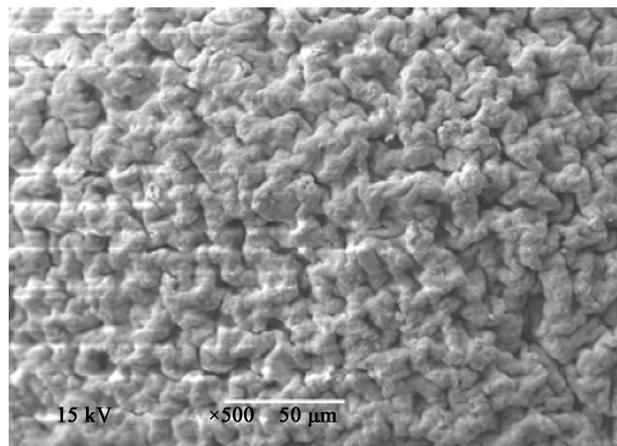
### 3. Results and Discussion

The observation of size, shape and surface topography of the dried CMMS are shown in **Figure 1**. The shapes of the dries microspheres were soherical, and the surface was rough, porous and unfolded. Furthermore the microsphere was not hollow.

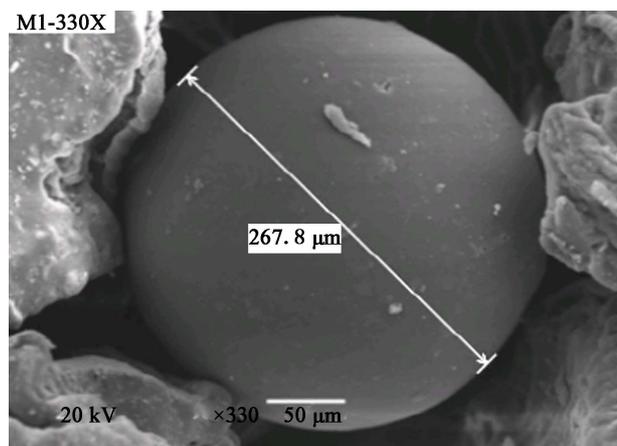
The particle size distribution curve (**Figure 2**.) showed sharp distribution range of microspheres, with 90% of spheres in size range of 1000-2600 nm with average particle size of 1800 nm and only 10% were oversized. The formed microspheres have uniform surface structure in which the microspheres lose their shape upon drying but regain them upon re-swelling. Which agreement with the results obtained by Erika Aranas *et al.* [26]. Erika Aranas *et al.* [26] prepared the spheres with technique similar to emulsion polymerization. Zhanga Ji *et al.* prepared composite magnetic microspheres based on artemisia seed gum and chitosan using the suspension cross-linking technique for use in the application of magnetic carrier technology [27]. Their results showed that composite



(a)



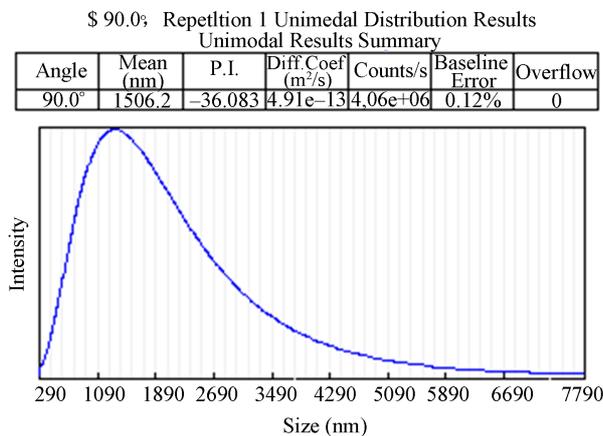
(b)



(c)

**Figure 1. SEM images of CMMS (a) CMMS with different size; (b) Rough surface of CMMS; (c) None hollow CMMS.**

magnetic microspheres can be produced in the size range 230 - 460  $\mu\text{m}$ .

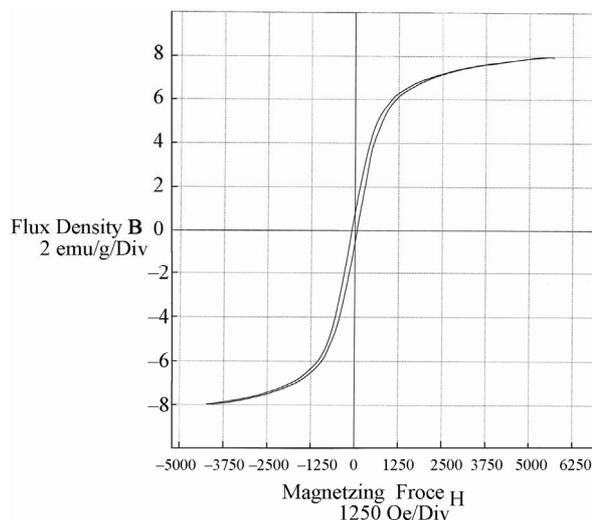


**Figure 2. Particles size distribution of CMMS with size range 1000 - 2600 nm.**

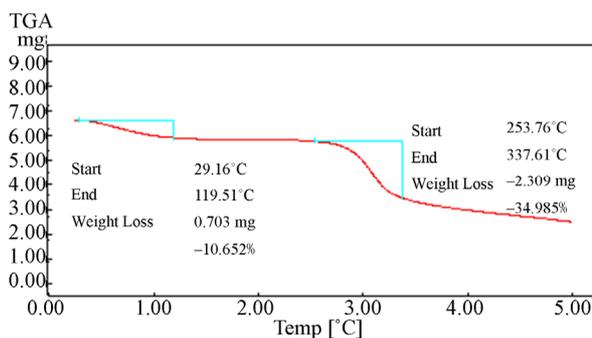
From the hysteresis loops of CMMS (**Figure 3**), the saturation magnetization was 8.065 emu/g, coercivity was 76.05 Oe and retentivity was 1.057 emu/g. These results are in agreement with Zhanga Ji *et al.* the magnetic properties of the composite magnetic microspheres were evaluated using a VSM [27].

The most effective parameters determining the magnetic properties were the stirring rate of the suspension medium and the Fe<sub>3</sub>O<sub>4</sub>/chitosan ratio, as in the case of the size/size distribution evaluation. The stirring rate of the suspension medium was varied between 500 and 1000 rpm for investigation of the effects of stirring rate on the magnetic properties of the composite magnetic microspheres. Furthermore, similar behavior for this parameter had been reported previously. Chiriac H. *et al.*, showed that the variation of the saturation magnetization and the coercive field as a function of the particle sizes for the atomized magnetic microspheres obtained for a diameter nozzle of 91 mm [28]. Their result showed that the saturation magnetization and the coercive field of the atomized microspheres with sizes between 26 and 300 mm range between 79.8 and 42 emu/g and 305 and 384 Oe, respectively.

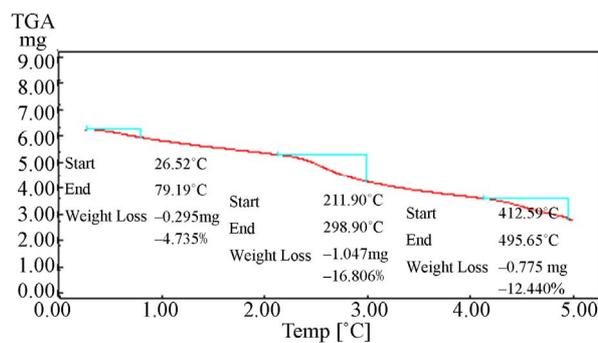
Thermal gravimetric Analysis (**Figure 4**) showed that the chitosan powder a small peak at 26°C - 106°C due to the volatilization of the solvent. Other strong transitions were found at 253°C - 337°C due to faster decomposition of chitosan powder. The difference in the thermal analysis between the two figures of chitosan powder and CMMS may be due to increase of thermal stability of magnetic microspheres than chitosan. This results in agreement with results obtained by Pich A. *et al.* [29]. Liu ZL *et al.* indicated that in their Thermal gravimetric Analysis of magnetic microspheres that the microspheres start degrading at about 260°C. The first mass loss is about 63% at the temperature between 260 and 280 1C,



**Figure 3. Hysteresis loop of CMMS.**



(a)

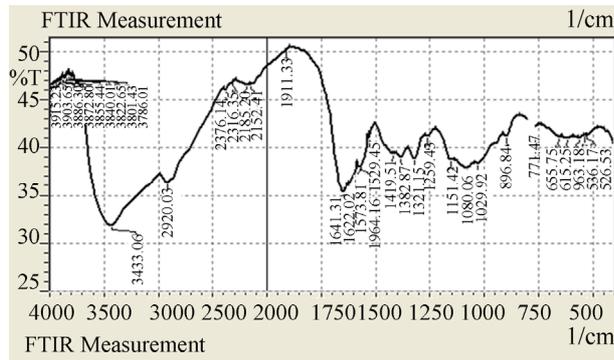


(b)

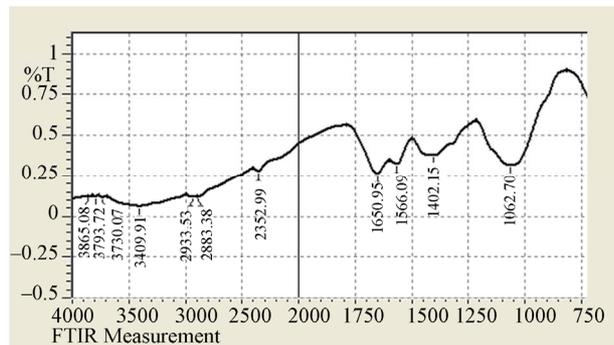
**Figure 4. Thermal gravimetric analysis of chitosan (a) and CMMS (b).**

and the second mass loss is about 10% at the temperature between 360 and 400 1C. The Tg is about 280 and 380 1C, respectively.

For the IR spectrum of chitosan (**Figure 5**) the characteristic absorption bands appeared at 3433 cm<sup>-1</sup> indicate to hydroxyl group, 1641 cm<sup>-1</sup> indicate to amide I, 1573 cm<sup>-1</sup> indicate amide II, 1382 cm<sup>-1</sup> indicate to am-



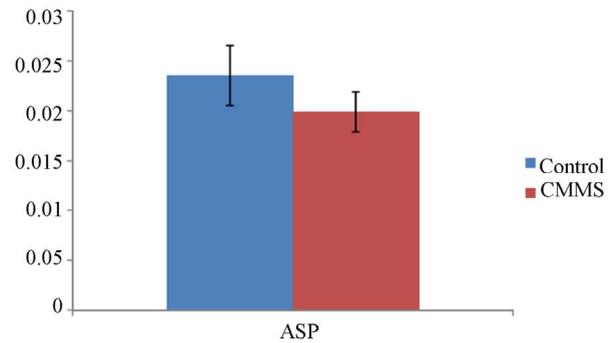
(a)



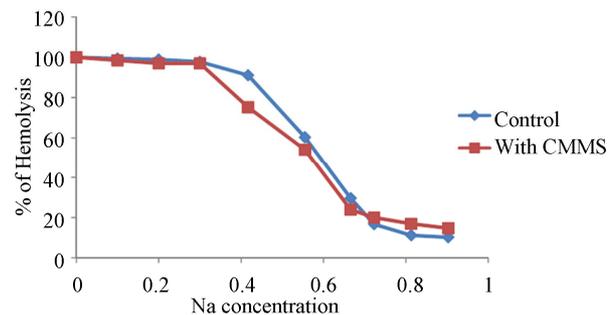
(b)

**Figure 5. the IR spectrum of chitosan (a) and CMMS (b).**

ide III, band at  $2920\text{ cm}^{-1}$  indicate to C-H stretching of copolymer, band at  $1029\text{ & }1080\text{ cm}^{-1}$  indicate to C-O stretching and band at  $1622\text{ cm}^{-1}$  indicate to  $\text{NH}_3$  absorption of chitosan. Compared with the spectrum of chitosan magnetic microsphere (**Figure 5**) the  $3433\text{ cm}^{-1}$  peak of hydroxyl group shifted to  $3409\text{ cm}^{-1}$  and a decrease in peak intensity of amid I ( $-\text{NH}_2$ ) group at  $1566\text{ cm}^{-1}$  which indicated the ionic cross-linking between amid I ( $-\text{NH}_2$ ) group of chitosan and  $-\text{C}=\text{O}$  groups of glutaraldehyde and new characteristic band appear at  $1650\text{ cm}^{-1}$  indicate to  $\text{C}=\text{N}$  group which indicate to cross-linking. The functional groups of materials are very important for diverse applications, especially for biotechnological purposes. Therefore, the present functional groups should be kept even if the shape (or geometry) is changed into a new form (*i.e.* microspheres or membrane). In this study the FT-IR of the spectra results obtained the peaks expected due to the geometry. In which the spectra of chitosan powder indicated the presence of the characteristic peaks such as hydroxyl group, amid-I, and amid-II, amid-III, and  $\text{NH}_3$  group. On the other hand the spectra of chitosan magnetic microspheres obtained shift in the characteristic peak of hydroxyl group and decrease in the peak intensity of amid-I due to the cross-linking between amid- and glutaraldehyde which



**Figure 6. ASP of erythrocytes incubated with CMMS compared to control.**



**Figure 7. Hemolysis of blood incubated with CMMS.**

obtained by the presence of characteristic peaks of  $\text{C}=\text{N}$  group. In the FTIR spectra of magnetic chitosan microspheres obtained by De-Sheng J *et al.* the (C), the peak was at  $3427\text{ cm}^{-1}$  corresponds to stretching vibrations of hydroxyl. The C-H stretching vibration of the polymer backbone is manifested through strong peak at  $2925\text{ cm}^{-1}$  and  $2855\text{ cm}^{-1}$  [30]. The stretch vibrations of C-O are found at  $1084\text{ cm}^{-1}$  and  $1032\text{ cm}^{-1}$ . For cross-linked chitosan microspheres, an additional peak at  $1656\text{ cm}^{-1}$  which corresponds to stretching vibrations of C-N bond. This peak indicates the formation of Schiff's base as a result of the reaction between carbonyl group of glutaraldehyde and amine group of chitosan chains. The little peak at  $1721\text{ cm}^{-1}$  shows the existence of independent aldehydic group in magnetic chitosan microspheres.

The erythrocytes incubated with CMMS showed lower values of ASP than control (uncubated erythrocytes) **Figure 6**. But the decrease in ASP was slightly small. This indicated that there was no harmful effect of CMMS on erythrocytes aggregation.

There was no difference in hemolysis curve between control and blood incubated with CMMS **Figure 7**. This make sure that CMMS have no harmful effect on blood.

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