

Macrostate and Microstate of EEG Spatio-Temporal Nonlinear Dynamics in Zen Meditation

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Abstract

Macrostate and microstate characteristics of interregional nonlinear interdependence of brain dynamics are investigated for Zen-meditation and normal resting EEG. Evaluation of nonlinear interdependence based on nonlinear dynamic theory and phase space reconstruction is employed in the 30-channel electroencephalographic (EEG) signals to characterize the functioning interactions among different local neuronal networks. This paper presents a new scheme for exploring the microstate and macrostate of interregional brain neural network interactivity. Nonlinear interdependence quantified by similarity index is applied to the phase trajectory reconstructed from multi-channel EEG. The microstate similarity-index matrix (miSIM) is evaluated every 5 millisecond. The miSIMs are classified by *K*-means clustering. The cluster center corresponds to the macrostate SIM (maSIM) evaluated by conventional scheme. Zen-meditation EEG exhibits rather stationary and stronger interconnectivity among frontal midline regional neural oscillators, whereas resting EEG appears to drift away more often from the midline and extend to the inferior brain regions.

Keywords

Electroencephalograph (EEG), Nonlinear Interconnectivity, Microstate, Macrostate, Zen Meditation

1. Introduction

Method based on the chaotic nonlinear dynamical modeling is developed to explore the *microstate* and macrostate phenomena of brain functioning. Instead of

characterizing the portrait of brain potential mapping at a time instant [1] [2], a *microstate* of the system could be viewed as an instantaneous snapshot of the nonlinear dynamical activities of all brain neurons in the millisecond scale. The microstate reveals the momentary glint of brain atlas in different physiological, psychological, or consciousness states [3]. The *macrostate* is characterized by the probability distribution of the statistical ensemble of all possible microstates. A *macrostate* can be viewed as the neuronal-dynamic equilibrium state of the macroscopic properties of the interregional (active/passive) activity distributed over a given time span. In brain dynamics, local neural networks collaborate together to accomplish specific tasks [4]. Each local neural-network module simultaneously plays the active (source) and passive (sink) role while sending and receiving electrical signals during the task. EEG measures the spontaneously aggregated electrical potentials generated by various types of neural oscillations of the brain down to millisecond-range temporal resolution. The brain dynamic macrostate becomes more spread out with the increase of various microstates during a time interval [5]. A microstate occurring with higher possibility indicates a better chance for the system to settle in such a specific microstate.

Scientific exploration has corroborated the effectiveness of meditation on health and well-being. Particular evidence includes the improvement of cardiovascular functions, immunity, and hormone regulation. Moreover, meditation makes positive changes in the brain, including the positive emotional states, better stress manipulation, enhanced mindful attention, noticeable reduction in anxiety and depression [6] [7] [8] [9]. Meditation is a unique state of transcendental consciousness beyond the ordinary mental process and consciousness. Most meditation practices are aimed to better manipulate the mind, brain function and physical state through mindfulness concentration and respiratory regulation. Having been adopted as the complementary medical practices, meditation inspired more scientific studies on its physiological and mental effects [10] [11] [12]. Meditation researches are mostly focused on Yoga and transcendental meditation from India, Japanese Zen, and Tibetan Buddhism [13] [14]. However, there is a lack of studies with respect to the orthodox heart-to-heart imprint sealing (HHIS) Zen meditation, of which the practitioners aim to liberate the true wisdom, *Bodhi*, inside the heart. HHIS Zen meditation was promulgated to mainland China by the 28th Zen patriarch Bodhidharma around AC 520 and transmitted to the current Zen patriarch Wu Jue Miao Tian. Patriarch Wu Jue Miao Tian for the first time disclosed the ten-mailuns system capable of effectively purifying the negative memories in the brain and converting the clinging brain into tranquil, detached brain [15]. It has been proposed that activation of ten mailuns locating at the glands or nerve plexuses can facilitate Zen meditation. HHIS Zen meditation, completely distinct from the other meditation techniques, follows the *heart-dominating* principle while meditations are mostly *mind-cultivating* practices. It is supposed that through years of Zen meditation, practitioners have their brain functions totally reformed into a so-called *detached* brain dominated by Bodhi. In this study, we investigate the Zen-medi-

tation EEG to objectively study the putative brain reformation process. EEG applications have become favorable since 1970s because of its advantages of good spatiotemporal resolution, economy, safety and convenience. Most of all, more scientific evidences of EEG variations have been obtained in different physiological, pathological, conscious and mental states in accordance with various temporal, spatial and spectral EEG characteristics [16] [17] [18] [19].

To explore the spatial interactions among local neural networks under Zen meditation, methods developed in nonlinear dynamical theory become more versatile and favorable [20] [21]. Brain dynamics can be conceived as a large ensemble of coupled nonlinear dynamical subsystems [22] [23] [24] [25]. We reported the nonlinear, chaotic characteristics of Zen-meditation EEG and disclosed significant nonlinear synchronization between EEG channels on a macroscopic scale [26]. This type of *nonlinear coupling* quantifying the nonlinear interdependence between different cortical areas provides a powerful mechanism for evaluating integrative neural processing [26]-[34]. This study presents a new scheme for probing into the microstate of nonlinear interconnectivity behaviors among various EEG channels and exploring the differences between Zen-meditation and normal resting EEG under the low-alpha oscillatory modes.

2. Methods

This paper was aimed at the concept and scheme of constructing the nonlinear interregional-interconnectivity microstate, of which the statistical property may be used to derive the corresponding macrostate. EEG data were collected in 2003 from 8 Zen-meditation practitioners (40 - 55 years old, Zen-meditation experience of 5 - 12 years) and 8 normal, healthy controls (20 - 30 years old). All subjects signed the Informed Consent Form before enrolling in the study and authorized the usage of their data for the scientific analysis. All procedures were consistent with the Declaration of *Helsinki* and were approved by the *Institutional Review Board* of National Chiao Tung University.

2.1. EEG Data

In the 45-minute recording, Zen practitioners practiced HHIS Zen meditation with all perceptions abiding inside the heart, while the control volunteers were awake *but* relaxed with eyes closed. EEG signals were recorded by PowerLab/16SP recording system (AD Instruments, Australia), using the 30-channel, common-reference (linked-mastoid MS1-MS2) electrode montage based on the international 10 - 20 system [26]. No particular intervention was applied. In each group, 15 segments of 1min low-alpha (~9 Hz) dominated EEGs were randomly, automatically selected by computer.

2.2. Signal Pre-Processing

The EEG signals were sampled at 200 Hz after being filtered by the analog band-pass filter (0.5 - 50 Hz). The segments contaminated by such artifacts as

eye blinking, eyeball movement and muscle activities were pre-screened. Please do not revise any of the current designations.

2.3. Nonlinear Interdependence Measure

The scheme for evaluating the nonlinear interdependence was based on the modified *algorithm* employed in computing the *similarity index* $\mathcal{S}(\mathbf{X}|\mathbf{Y})$ [26]. Major tasks in the algorithm involve reconstruction of the m -dimensional phase-space trajectory and computation of the average cloud radius centered at a given state point.

In the phase-space reconstruction, the brain is considered as the nonlinear dynamical system. State variables \mathbf{X} and \mathbf{Y} in the m -dimensional phase space are constructed respectively from two channels of EEG signals $x[i]$ and $y[i]$ by Takens embedding theory [23], $\mathbf{X} = \{X_i | X_i = (x[i], x[i + \tau], \dots, x[i + (m - 1)\tau])\}_{i=1}^N$. The reconstruction assumes a total number of N system-state points in the m -dimensional phase-space trajectory, utilizing a rational time delay τ (in sample). The dimension m indicates the number of degrees of freedom of the nonlinear system and, accordingly, reflects the *complexity* of the system dynamics.

To compute the average cloud radius, consider a state point X_i on the m -dimensional phase trajectory. As illustrated in **Figure 1**, a KNN hypersphere, formed by the K 's nearest neighbors (KNNs) of X_p , is a cloud composed of K neighboring points around X_p .

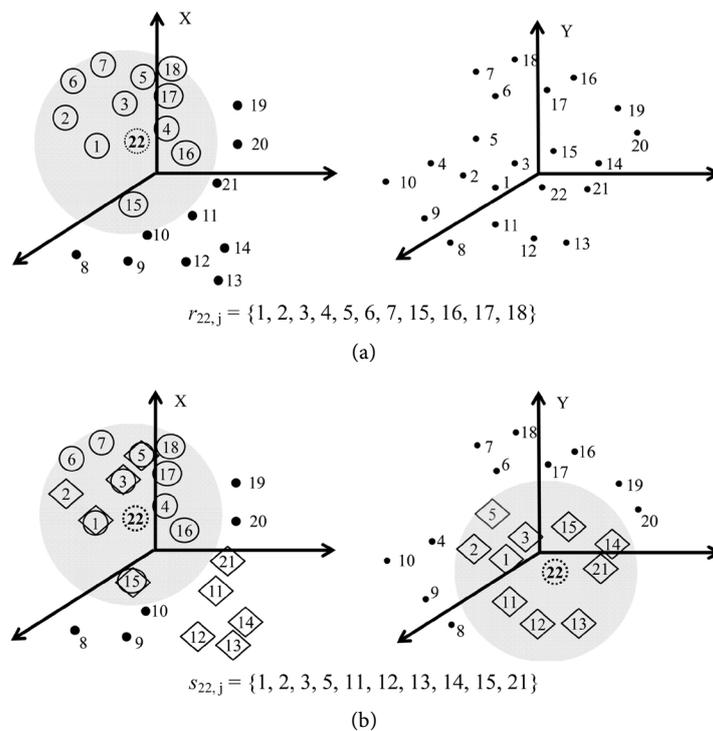


Figure 1. Illustration for (a) left: Self neighbors $X_{22,j}$ (○), and right: State points in Y, (b) left: Mutual neighbors $X_{s_{22,j}}$ (◇) where the indexes $s_{22,j}$ are determined from the indexes of KNN of Y_{22} ($K = 10$), assuming $m = 3$, $K = 10$, $i = 22$, and $N = 22$.

Let $r_{i,j}$ and $s_{i,p}$, $j = 1, \dots, K$, denote the time indices of the K NN points of X_i and Y_p respectively. Note that $r_{i,j}$ and $s_{i,j}$ must be no greater than i for a causal processor. Then, the set of state points in the K NN hypersphere centered at X_i is $\{X_{r_{i,j}} | j=1, \dots, K\}$. The average square Euclidean distance from X_i to its K NN neighbors (or the average square radius of the cloud centered at X_i) is defined as:

$$R_i(\mathbf{X}) = \frac{1}{K} \sum_{j=1}^K \|X_i - X_{r_{i,j}}\|^2 \quad (1)$$

where $\|\cdot\|$ indicates the operator for calculating the Euclidean distance. Another point cloud around X_i is formed with respect to its *mutual* neighbors $X_{s_{i,j}}$, which share the same temporal indexes of the K NN of Y_p . In this sense, the \mathbf{Y} -conditioned average square Euclidean distance is defined by replacing the true nearest neighbors of X_i by the *mutual* neighbors [26]:

$$R_i(\mathbf{X}|\mathbf{Y}) = \frac{1}{K} \sum_{j=1}^K \|X_i - X_{s_{i,j}}\|^2 \quad (2)$$

In the extreme case of $K = N$, the average square radius of the cloud centered at X_i becomes

$$R_i^N(\mathbf{X}) = \frac{1}{N-1} \sum_{j=1, j \neq i}^N \|X_i - X_j\|^2 \quad (3)$$

Then, for two strongly synchronized systems, both self and mutual neighbors mostly coincide so that $R_i(\mathbf{X}) \approx R_i(\mathbf{X}|\mathbf{Y}) \ll R_i^N(\mathbf{X})$; whereas for independent systems, mutual neighbors are more scattered that leads to

$R_i(\mathbf{X}) \ll R_i(\mathbf{X}|\mathbf{Y}) \approx R_i^N(\mathbf{X})$. Accordingly, the degree of interdependence of these two systems is quantified by the *similarity index* S [26] between these two cloud patterns formed by self and mutual neighbors, as defined below:

$$S(\mathbf{X}|\mathbf{Y}) = \frac{1}{N} \sum_{i=1}^N \frac{R_i(\mathbf{X})}{R_i(\mathbf{X}|\mathbf{Y})} \quad (4)$$

The average over the entire data points in the m -dimensional phase space trajectory can be referred as the *macrostate* similarity index (maSI). Accordingly, the microstate similarity index (miSI) at a specific time instant i can be defined as the ratio of the average square cloud radius to the average square \mathbf{Y} -conditioned cloud radius. That is

$$S_i(\mathbf{X}|\mathbf{Y}) = \frac{R_i(\mathbf{X})}{R_i(\mathbf{X}|\mathbf{Y})} \quad (5)$$

$S(\mathbf{X}|\mathbf{Y})$ assesses the statistical dependence of the state-space structure of \mathbf{X} on that of \mathbf{Y} in the sense of testifying whether closeness in \mathbf{X} implies closeness in \mathbf{Y} and vice versa. Two identical systems with the same sets of self and mutual neighbors result in the maximum similarity index ($S = 1$); whereas the index is close to zero ($S \approx 0$) for completely independent systems. The opposite interdependence ($S(\mathbf{Y}|\mathbf{X})$) can be computed analogically. Notice that similarity indexes are in general asymmetric, that is, $S(\mathbf{Y}|\mathbf{X}) \neq S(\mathbf{X}|\mathbf{Y})$. $S(\mathbf{X}|\mathbf{Y})$ evaluates the effect of system \mathbf{Y} on system \mathbf{X} . From the point of view of the system theory, signal \mathbf{Y} is

regarded as the *source* or the active role in the interaction; while signal \mathbf{X} plays a passive role (a *sink*). On the other hand, $S(Y|X)$ analysis considers \mathbf{Y} as the *sink* that plays the passive role [22].

The asymmetry of S is one of the main advantages over the other nonlinear measures such as the mutual information and the phase synchronizations. The fact that S is asymmetric allows us to study not only topographic patterns but also functional properties. By considering each EEG electrode either as a sink or as a source in the nonlinear-interdependence interaction, we may thereby further explore the brain functional topological profile and the direction of interaction among local neuronal networks [17]. For example, the condition of $S(Y|X) > S(X|Y)$ indicates that \mathbf{Y} depends more on \mathbf{X} than vice versa. In other words, \mathbf{X} is said to be more *active* and \mathbf{Y} is more *passive*. By considering each electrode either as a sink or as a source in the nonlinear dynamical interaction, we may explore the spatial direction of the interaction and the dominance of local neuronal networks under Zen meditation [35].

To determine the implementation parameters, we employed mutual information function in determining the appropriate time delay. The suitable range of τ is 5 - 7 samples. Embedding dimension m can be determined by the convergent estimate of dimension. To ensure the completeness of system dynamics, the suitable range of m is 8 - 10 using Cao's method to explore the system dynamics under various m 's. There is no analytical approach for determining the value of K in constructing the K NN hypersphere. When K is small ($K \leq 4$), the neighborhoods in one reconstructed trajectory can map into the other perfectly. The strength of nonlinear interdependence between two EEG trajectories is so strong that S values are close to 1. Likewise, if K is large enough to cover the most points in phase space, it causes strong strength of nonlinear interdependence since the X -neighbor and X/Y -mutual neighbor cloud radii overlap with each other. Values of K ranging from 5 to 20 lead to a consistent estimate of similarity index. To reduce the computational load, $K = 6$ is adopted. The window length N is selected to encompass the stabilization of dynamical behavior in the sense of the convergent estimate of EEG nonlinear dynamical property. The window of 2 - 5 seconds was applied previously when studying the macroscopic behavior. To explore the microstate nonlinear dynamics of brain functioning, the window size of 1 second (200 samples) is adopted. Note that the 1-second window is the K NN searching range in (1) and (2), indicating the influence of past events on current system state. The miSI in (5) is computed every 0.005 second for a given cluster center. Finally, the implementing parameters were: $\tau = 6$ (sample points), $m = 8$, $K = 6$ and $N = 200$ [26] [36].

2.4. Microstate SIM Clustering

Interpretation of long-term, multichannel EEG record has been one of the most important tasks in investigating the time-varying brain dynamics under the specific physical, mental, conscious, or cognitive states. Before interpreting the EEG record, the first step is normally to identify the possible brain dynamical charac-

teristics modeled by specific representations, mostly in quantitative form. Different representations are designed to emphasize different brain behaviors including spatial-temporal focalization of EEG rhythms, topographical mapping of cortical potentials, efficiency of inter-regional neural-network interactions, etc. Such problem is referred to the area of knowledge discovery in databases (KDD), or data mining.

Among various clustering methods, K -means clustering based on minimizing a specified objective function might be the most widely used method [37]. K -means clustering classifies the n elements into k sets, $\mathbf{S} = \{S_1, S_2, \dots, S_k\}$ by way of minimizing the within-cluster sum of squared differences between each element and the cluster's center:

$$\delta = \sum_{i=1}^k \sum_{x_j \in S_i} (x_j - m_i)^2 \quad (6)$$

where center m_i is the average of the elements in the i th cluster S_i . Iterative refinement technique is implemented. Given an initial set of k centers m_1, m_2, \dots, m_k . The algorithm proceeds by alternating between two steps, *classification* and *updating* step. In classification step, each element (x_p) is assigned to the cluster of which the center is closest to x_p .

$$S_i^{(t)} = \left\{ x_p \left\| \|x_p - m_i^{(t)}\|^2 \leq \|x_p - m_j^{(t)}\|^2, \forall j, 1 \leq j \leq k \right\} \right\} \quad (7)$$

where t is the number of iteration. In updating step, the new cluster centers $\{m_i, 1 \leq i \leq k\}$ are calculated as below.

$$m_i^{(t+1)} = \frac{1}{N_{i,t}} \sum_{x_j \in S_i^{(t)}} x_j \quad (8)$$

where $N_{i,t}$ is the number of elements in the cluster i at the t^{th} iteration. The algorithm converges when the classification settles, that is, no more alteration of cluster elements.

Microstate similarity index (miSI) computed by (5) is evaluated for all 30×30 EEG channel pairs from which we form the miSIM (microstate similarity index matrix). All the miSIMs in a given time interval (one minute, in this study) are classified by K -means clustering algorithm. Totally 12,000 miSIM features in one-minute EEG are classified into five clusters by K -means clustering. The final step is to screen out approximately 30% of the feature vectors which are too far away from each cluster center. The final cluster centers are computer by averaging all the miSIMs inside the cluster. The average miSIM is simply the sum of all miSIMs divided by the total number of miSIMs in the specified pool.

2.5. Macrostate SIM

The center of each cluster is the macrostate SIM (maSIM) of the miSIM cluster. We discovered the maSIM of the largest cluster could represent the SIM derived from the conventional method [26] in (4). The advantage of analyzing microstate SIM is to access the flashlight transient behavior of brain dynamics down to

the millisecond scale. The cluster centers may be used as the feature bases (templates) to interpret the nonlinear interdependence microstates of long-term EEG record. Each miSIM is classified into the cluster of which its center is nearest to the miSIM. **Figure 2** displays the template of maSIM, with each row (column) indicating the efficacy of the passive (active) role of the channel on the vertical (horizontal) coordinate.

2.6. Connectivity Plot

We designed the connectivity plot to demonstrate the dominant interconnectivity strength among inter-regional neural networks. The connectivity plot also reflects the lateral and longitudinal symmetrical property. The major scheme is to connect two EEG electrode sites with a line if the source-role miSIM \geq threshold (0.6). To make the plot more informative and versatile, different line forms and colors may be used to indicate the spatial relation. In the longitudinal connectivity plot (LCP), EEG channels are divided into frontal (Fp1, Fp2, F7, F3, Fz, F4, F8, FT7, FC3, FCz, FC4, FT8), central (T7, C3, Cz, C4, T8), and posterior (TP7, CP3, CPz, CP4, TP8, P7, P3, Pz, P4, P8, O1, Oz, O2) groups. In the transversal connectivity plot (TCP), EEG channels are divided into left (Fp1, F7, F3, FT7, FC3, T7, C3, TP7, CP3, P7, P3, O1), right (Fp2, F4, F8, FC4, FC8, C4, T8, CP4, TP8, P4, P8, O2), and midline (Fz, FCz, Cz, CPz, Pz, Oz) groups. LCP emphasizes the longitudinal relationship, whereas TCP reflects the dominant connectivity between two hemispheres. The LCP and TCP provide the profile of high

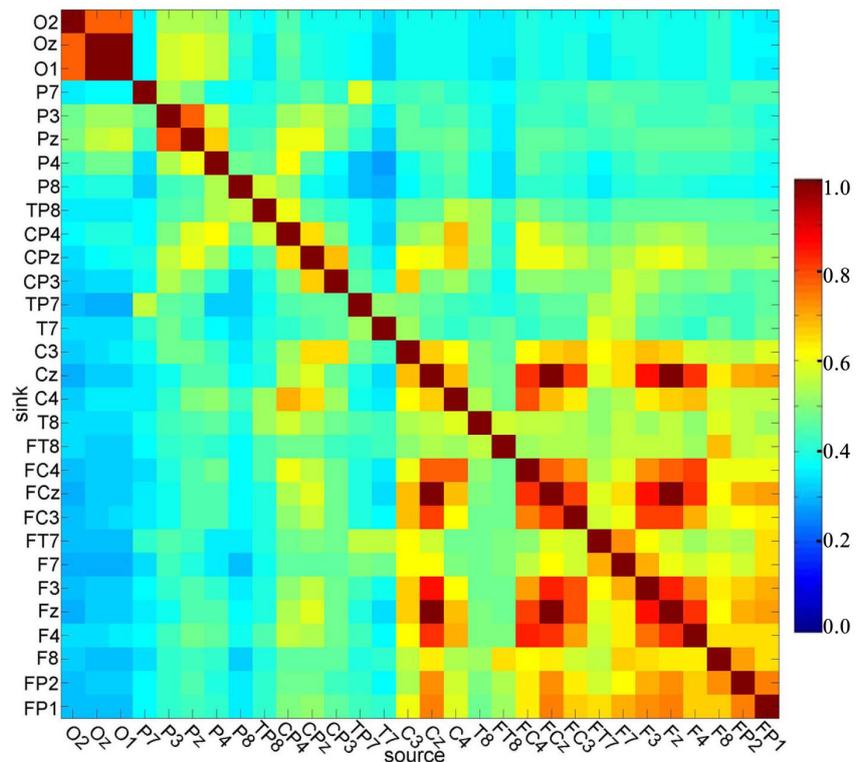


Figure 2. MaSIM template (the second cluster center for Zen-meditation EEG).

interdependence ($SI \geq 0.6$) for channel pairs with the frontal-posterior and left-right relation. Red (blue) lines in LCP indicate the source locates in the frontal (posterior) region, while green lines mark the strong interdependence of channel pairs with the source on the transversal line (T3-C3-Cz-C4-T4). In the TCP plot, red (blue) lines indicate the source locates in the right (left) hemisphere, while green lines indicate the source locates in the midline.

3. Results

The miSIMs for one-minute Zen-meditation and resting EEG are classified into five clusters. **Figure 3** and **Figure 4** displays the cluster centers (last row) and 3 sampled cluster members (miSIMs, on the top three rows) in each of the five clusters, respectively, for Zen-meditation EEG and resting EEG. The probabilities of occurrence of each individual cluster are 13.6% (16.4%), 11.5% (10.2%), 23.8% (28.0%), 30.4% (32.5%) and 20.7% (12.9%) in a 5-minute Zen-meditation (resting) EEG. The second cluster appears least often in both EEG cases, nevertheless, contains the most active miSIMs. The most inactive miSIMs are in the first (fifth) cluster for Zen-meditation (resting) EEG.

In **Figure 3** and **Figure 4**, all clusters contains the frontal-central focalized (channels Cz, FCz, Fz) miSIMs. The miSIMs in the first and fifth clusters exhibit comparably suppressed inter-channel activities. The second cluster contains the most active regional interconnectivity of miSIMs, with the activity in the centro-parietal regions increasing moderately. In the third cluster, spatial characteristic of higher interdependence is very similar to which of the first cluster. Nevertheless, miSIMs in the third cluster have larger regions of mid-level ($0.3 \leq$

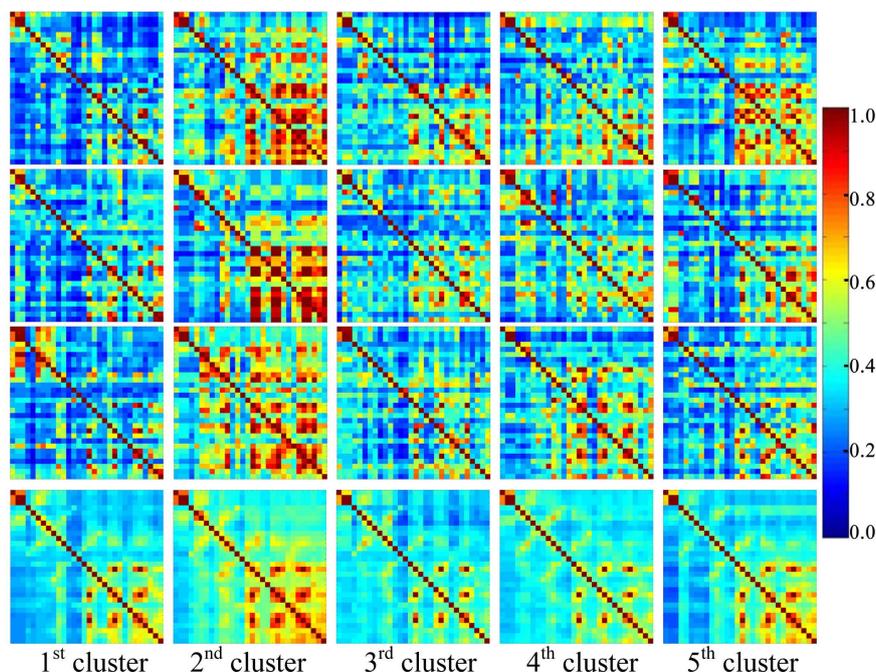


Figure 3. Rows 1 - 3 display 3 sampled miSIMs in each of the five clusters for Zen-meditation EEG, the last row display the corresponding cluster centers (maSIMs).

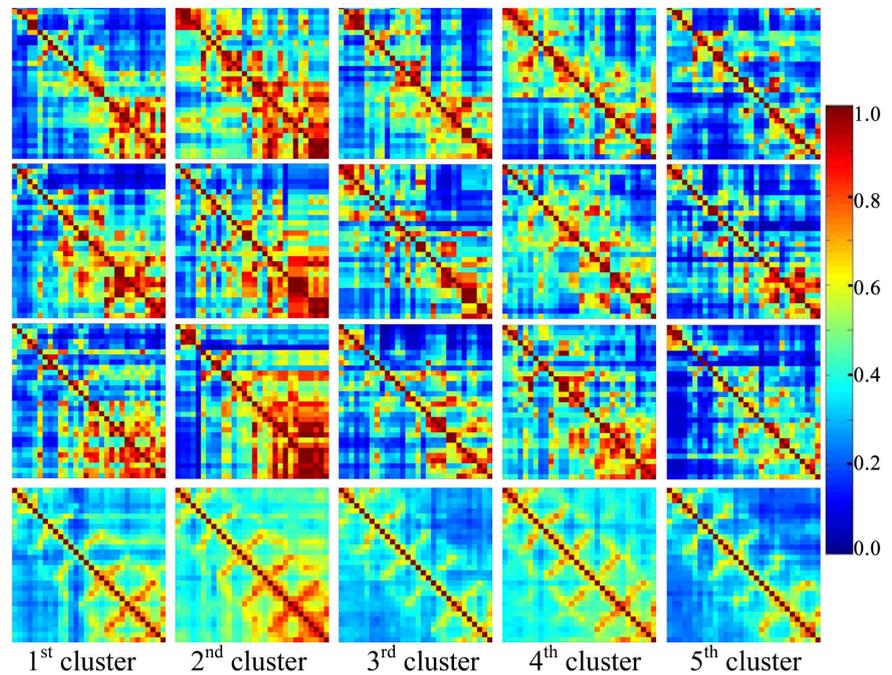


Figure 4. Rows 1 - 3 display 3 sampled miSIMs in each of the five clusters for resting EEG, the last row display the corresponding cluster centers (maSIMs).

$SI \leq 0.5$, light blue in **Figure 3**) strengths of interdependence. The dynamics of nonlinear interdependence of the fourth cluster is more vigorous than which of the first and the third cluster, yet, is inactive compared with the second cluster possessing highest extending capability in the frontal channels. The overall nonlinear interdependence of the fifth cluster is similar to which of the fourth cluster in the frontocentral regions, yet, becomes more inactive in the temporo-parietal and occipital regions.

Zen-meditation EEG exhibits right-dominant, while resting EEG does not. The active regions of resting EEG (with $SI > 0.6$, in the connectivity plots) are more dispersive that extend to inferior frontal and temporal cortexes. Comparison of **Figure 3** and **Figure 4** reveals that Zen-meditation brain exhibits rather constraint, localized characteristics of regional interconnectivity, while normal brain at rest tends to extend the strength of influence to other regional neural networks. Moreover, resting EEG demonstrates the remarkable expansion of source-driven effect towards the inferior brain regions (EEG channels F7, F8, FT7, FT8, T7, T8, TP7 and TP8). The phenomenon may be clearly illustrated by connectivity plots (LCP and TCP) in **Figure 5**.

Table 1 lists the averages of source-role (active) miSIMs in 5 brain regions for each cluster (Zen-meditation/resting EEG). Regional average smears out the statistical difference between two groups ($p < 0.05$ only for cluster 5). The largest microstate SI average appears in the right frontal (0.549) and central (0.568) region (the 2nd cluster) for Zen-meditation EEG; while the smallest value appears in the left posterior region (0.327 in the first cluster and 0.349 in the fifth cluster). Notice that, among all five clusters, right hemisphere always exhibits higher

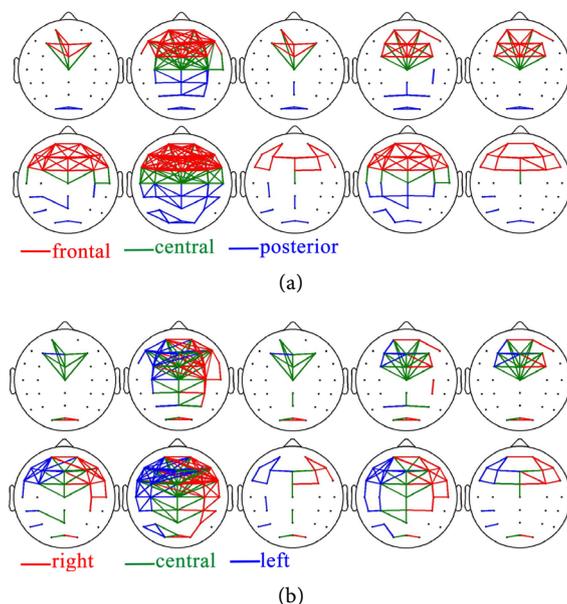


Figure 5. (a) LCP and (b) TCP for Zen-meditation EEG (top) and resting EEG (bottom).

Table 1. Averages of source-role (active) miSIMs in 5 brain regions for each cluster (Zen-meditation/resting EEG).

Cluster Brain region	1	2	3	4	5
Left Frontal	0.37/0.46	0.53/0.57	0.39/0.40	0.45/0.47	0.44/0.37
Right Frontal	0.39/0.47	0.55/0.57	0.40/0.39	0.46/0.47	0.45/0.37
Central	0.42/0.43	0.57/0.55	0.45/0.40	0.50/0.47	0.47/0.36
Left Posterior	0.33/0.33	0.44/0.46	0.37/0.38	0.41/0.42	0.35/0.32
Right Posterior	0.35/0.37	0.46/0.46	0.39/0.37	0.42/0.42	0.36/0.31

interdependence strength than left hemisphere, regardless of the frontal or posterior region. Such a right-dominant behavior is apparent in the second cluster (**Figure 5(b)**). In respect of the longitudinal relation, the frontal region apparently dominates over the posterior region in both left and right hemispheres for all the five clusters.

In resting EEG, the largest miSIM average appears in the right frontal (0.570) and left frontal (0.574) region (the 2nd cluster); while the smallest value appears in the posterior region (0.317 in the left posterior and 0.312 in the right posterior, both belonging to the fifth cluster). With respect to the lateral symmetry, there exists no consistent laterally dominant behavior among all five clusters, unlike the right dominant characteristics in all five cluster centers for the Zen-meditation practitioner. With respect to the longitudinal relation, the frontal region apparently dominates over the posterior region in both left and right hemispheres for all the five clusters.

Zen-meditation miSIM appears to be more localized with the major activity in the midline (Fz, FCz, and Cz). On the other hand, rest miSIM is more outspread with the major activity extending to inferior brain area. We compare the miSIMs

in the 4th cluster between Zen-meditation and resting EEG since the 4th cluster is the largest cluster. **Figure 6** illustrates the brain mappings of miSIMs, in the 4th cluster, of Zen-meditation (left) and resting (right) EEG given the source locating at channel: (a) C3, (b) Cz, (c) F8, (d) P3, and (e) T8.

4. Discussion

Figure 6 demonstrates noticeable distinction between Zen-meditation and rest EEG (p value $\ll 0.05$) although they both are mainly composed of low alpha (8 - 10 Hz) activities. Channels C3 and C4 are in charge of sensorimotor integration for the right and left body. While entering into deep Zen meditation, practitioners transcend the time-space perception and cognition. Channels P3 and P4 associated with spatiotemporal information processing of right half and left half of space appear to be inactive for Zen-meditation practitioners. Brain function near EEG channel F8 correlates with emotional expression. In addition, remarkable distinction of spatially nonlinear interconnectivity was observed at temporal lobe (**Figure 6(e)**) correlating with auditory processing. Zen-meditation practitioners having activated ChanXin mailun (inside the third ventricle) are able to focalize the brain activities within the smaller regions around the midline. Channels Fz, FCz and Cz interact tightly (**Figure 6(b)**). Accordingly, practitioners can easily transcend the interference from sensory organs and emotions. Other channels beyond the midline region are much quieter for Zen-meditation practitioners, yet, are rather vigorous for the normal people at rest.

5. Conclusions

This paper reports a novel scheme of investigating the microstates of spatially nonlinear interdependence among EEG channels. Previous researches have been focused on the macrostate analysis of EEG nonlinear interdependence [22] [32]. Averaging the raw SI's (similarity indexes) over an epoch of (for example, 2 seconds) results in the obscurity of possibly important regional neural-network interactions. Microstate analysis down to millisecond scale allows us to explore

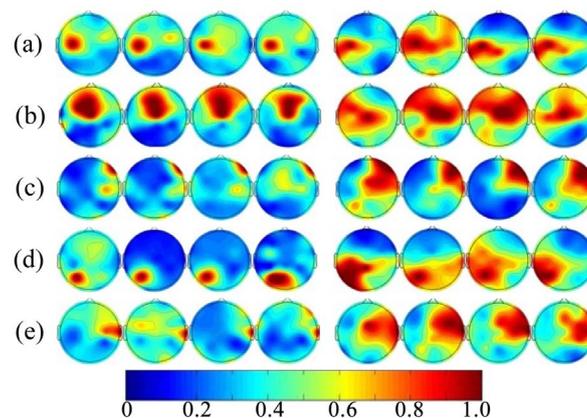


Figure 6. Brain mappings of active miSIMs for (left) Zen-meditation EEG, and (right) resting EEG, assume the source channel is (a) C3; (b) Cz; (c) F8; (d) P3 and (e) T8.

microscopic transient behaviors. As illustrated in **Figure 7**, brain mappings of maSIMs, in the 4th cluster, reveal slight difference between Zen-meditation EEG (left) and resting EEG (right). Nevertheless, macrostate SIM is deficient in expressing the transient dynamics of time-varying interregional connectivity in comparison with microstate SIMs in **Figure 6**. Student T-test shows statistically significant difference in maSIMs (**Figure 7**) between Zen-meditation and resting EEG (p value < 0.05).

The analysis found significant differences of interregional-connectivity microstates between Zen-meditation EEG and resting EEG, particularly in the regions known to be involved in sensorimotor function, cognitive and spatial perceptions, emotion and mood regulation, and verbal and auditory processing. In preparation for entering true Zen realm, brain needs to switch to the *detached* state so that the spiritual heart starts to take over. Zen practitioners accomplish such a conversion by simultaneously abiding in the third ventricle of the brain, the heart, and the perineum [18] [38] which leads to the so-called Heaven-Man-Earth harmonious resonance in Zen. The concrete, tight connection among Fz, FCz and Cz (**Figure 6(b)** left) provides the evidence of the effect of tri-mailuns unification. Brain in such a state is totally tranquil and peaceful, being relieved from the routine processing of the external messages from sensory organs and void of all the wandering thoughts, cognitions, or mental activities. Somehow this finding is resonating with papers on EEG effects of meditation, though using different mediation techniques [39].

In comparison of the results, Zen-meditation miSIM appears to be more focused in the midline (Fz, FCz, and Cz), whereas resting miSIM is more outspread with the major activity extending to inferior brain regions. Zen-meditation miSIM has higher interdependence only in a smaller area mainly in the fronto-central region (Cz-F3: 0.76, Cz-F4: 0.71, FCz-F3: 0.77, FCz-F4: 0.71). Resting miSIM has higher regional interdependence in the electrode pairs of nearby EEG channels, particularly in the fronto-temporal regions (FT7-T7: 0.67, FT8-T8: 0.61, FC3-C3: 0.62, FC4-C4: 0.63). In addition, resting miSIM has more activities in the occipital region. Comparing the miSIM cluster with the lowest activity (1st for Zen-meditation EEG and 5th for resting EEG), Zen-meditation miSIM has very low activity outside the fronto-central region (Cz, FCz and Fz), while resting miSIM still involves significant activities in such regions like F7, F8, F3 and F4, as illustrated in **Table 2**. The T test shows statistically significant difference between two groups with $p < 0.05$.

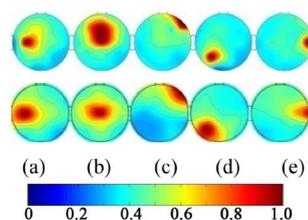


Figure 7. Brain mappings of maSIMs of Zen-meditation EEG (up) and resting EEG (down) assume the source channel is (a) C3; (b) Cz; (c) F8; (d) P3; and (e) T8.

Table 2. Averages of microstate similarity indexes of the specified channel pairs in the 1st cluster for Zen-meditation EEG and which in the 5th cluster for resting EEG.

Channel pairs	Zen meditation	Resting	Channel pairs	Zen meditation	Resting
F7-FT7	0.49	0.79	F8-FT8	0.53	0.75
F7-F3	0.47	0.66	F8-F4	0.49	0.74
F7-Fp1	0.44	0.74	F8-Fp2	0.56	0.8
F3-FC3	0.57	0.77	F4-FC4	0.54	0.75
F3-F7	0.51	0.67	F4-F8	0.51	0.75
F3-Fp1	0.59	0.78	F4-Fp2	0.50	0.78

In the results of analyzing Zen-meditation EEG, profoundly experienced practitioners, after the ignition of ChanXin inside the third ventricle, reveal macroscopic behaviors of brain dynamics with a remarkable stationary oscillation mode among all regional neural oscillators that have been tuned in with the particular resonance via heart-to-heart imprint practice in Zen meditation. On the other hand, microscopic activities involve subtle transitions of effectiveness among regional neural oscillators, in our hypothesis, to modulate the brain neural dynamics for reducing the mental activities, cleansing the subliminal consciousness, and transcending the time- and space-dependent physical world.

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