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## **Image Noise Analysis of a Large Ring PET** Scanner

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## Abstract

Image noise analysis of a large ring PET scanner "macro PET" performed using two different phantoms, namely a Jaszczak SPECT phantom and a uniform cylindrical phantom. In the present work, simple 2D filtered back projection was used to reconstruct all the images, and in almost all the cases a Hamming filter of cutoff frequency 0.4 and a 256 by 256 matrix with zoom factors from 1 to 4 were used in order to investigate the imaging capabilities of the new scanner and the influence of filter and cut-off frequency on the filtered back projected images. Results indicate that 11.1 mm cold rod in the Jaszczak phantom images can consistently be seen. The Coefficient of variation (CV) results for Hann and Hamming filters are very similar and increase approximately in linear fashion with higher cutoff frequency. The value of CV for the Parsen filter is lower than the value for Hann and Hamming filters. It concludes that all filters with low cut off-frequency (<0.6) would suppress image noise but decrease contrast.

## **Keywords**

PET, Sinogram, Filter & CV

## 1. Introduction

Positron emission tomography (PET) is a powerful radiotracer imaging technique, in which the distribution of radiolabelled tracer molecules in a patient is measured by detecting pairs of back-to-back gamma rays produced in positron-electron annihilation. This functional imaging technique has been used for the last few decades in many clinical applications [1] [2] such as the detection and diagnosis of malignant carcinoma [3], in monitoring response after therapy [4].

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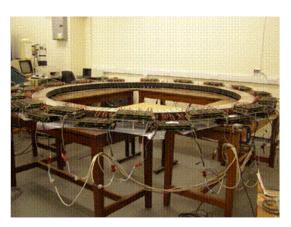


Figure 1. A photograph of the macro PET system [5].

The large ring PET scanner "macro PET" (**Figure 1**) with an inner diameter of 2.34 m was created by reconfiguring components from an original ECAT 951 [6]. The original system has 32 detector modules ("buckets") mounted in two rings with an inner diameter of 100 cm and a 10.8 cm axial FOV.

The original system is based on bismuth germanate (BGO) block detectors. Each block consists of a BGO crystal  $50 \times 60 \times 30$  mm<sup>3</sup>, backed by four photomultiplier tubes (PMTs). The front of the crystal is cut into an  $8 \times 8$  array of crystal elements, each  $6.25 \times 6.75$  mm<sup>2</sup>. The blocks are grouped into buckets each comprising four detector blocks together with their associated electronics (preamplifiers and discriminators) under the control of a microprocessor. Data from all the buckets are fed to a set of coincidence processors which identify events in which a pair of 511 keV *y*-rays have been detected in two buckets within the system resolving time of 6 ns. For the new large ring system "macro-PET", the detector blocks have been remounted in a single horizontal ring of 128 blocks.

A delayed timing window was used to record the distribution of random coincidences. Data were initially recorded in histograms (prompt minus delayed events) appropriate to the image planes of the original geometry and were then rebinned into the correct sinograms for the new geometry. In this rebinning the gaps between blocks were allowed for by treating each large ring as if it consisted of  $1152\ (128\times 9)$  crystal elements with every ninth detector absent, and interpolation was used to complete the missing sinogram elements. Arc correction of the projection data was achieved by performing a further rebinning with linear weighting.

The influence of filter and cut-off frequency on the filtered back projected image noise and contrast were investigated. The noise level was investigated by computing the coefficient of variation (CV) from the reconstructed image for a uniform cylindrical phantom in no-septa configuration.

## 2. Materials and Method

Imaging studies were performed using two different phantoms, namely a Jaszczak SPECT phantom, a uniform cylindrical phantom. Events within the

energy window from 250 keV to 850 keV were accepted from the system. Simple 2D filtered back projection has been used to reconstruct all the images presented here, and in almost all the cases a Hamming filter of cutoff frequency 0.4 and a 256 by 256 matrix with zoom factors from 1 to 4 were used. Different filter window functions and a range of cut-off frequencies were considered with filtered back projected images for this study.

## 2.1. Jaszczak SPECT Phantom

The Jaszczak SPECT phantom (Deluxe) is often used for assessing the image quality in nuclear medicine images. It consists of a cylinder with perspex inserts which create cold lesions when the phantom is filled with radioactive solution. In the present work, a Jaszczak SPECT phantom with interior dimensions of 21.6 cm long and 18.6 cm in diameter was used, containing six solid (perspex) spheres of different sizes located in the upper section and six different sets of cylindrical rods in the lower section. The cold rod dimensions are 4.8 mm, 6.4 mm, 7.9 mm, 9.5 mm, 11.1 mm, 12.7 mm.

The data were obtained in no-septa mode by filling only the lower half of the phantom with approximately 2.5 litres of water, and adding approximately 200 MBq of 18-F. Data were acquired for 600 s per image, with the phantom mounted at the centre of the field of view and at different radial offsets. Each image was reconstructed using filtered back projection and incorporating the calculated attenuation correction for a water-filled cylinder. Different values of cutoff frequency (expressed as a fraction of the Nyquist frequency) were applied to each filter window function.

## 2.2. Uniform Phantom

Two types of uniform cylindrical phantom containing short (18-F, t1/2=109.8 min) and long half life (68-Ge, t1/2=270.8 d) sources were used. In both cases, the uniformity and noise level of the reconstructed images were investigated by computing the coefficient of variation (CV).

#### 2.2.1. Short Half Life Uniform Phantom

The short half life uniform phantom was prepared from a 20 cm diameter cylindrical phantom with an axial length of 20 cm filled with 18-F solution only to the depth of the FOV.

## 2.2.2. Long Half Life Uniform Phantom

Noise level in the reconstructed image was measured by calculating coefficient of variation (CV) using data from a 68-Ge uniform 20 cm diameter cylindrical phantom with an activity of 5 MBq. The source was positioned at the centre of the scanner field of view (FOV), and the projection data were acquired for 18 hrs. The total number of acquired coincidence events was 45 M which includes 1.7% randoms. The coefficient of variation was computed as the ratio of the standard deviation to the mean pixel counts ( $\sigma/\mu$ ) over a region of interest (ROI) on the filtered back projected image. The ROI on the image plane was drawn in

the same area with a radius of 2 cm for each case.

## 3. Results and Discussion

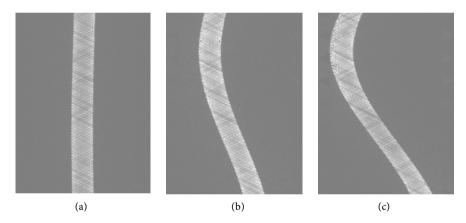
## 3.1. Sinograms at Different Radial Positions

Sinograms produced by imaging the Jaszczak SPECT phantom at three locations inside the system are presented in **Figure 2**.

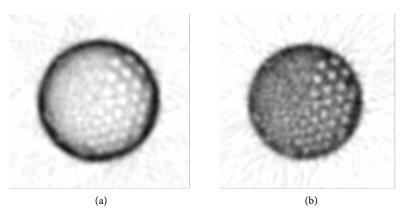
The results indicate that the sinograms produced by positioning the phantom at the scanner centre are consistently good. Sinograms are distorted as radial offset increases due to the variations of LOR spacing. This distortion was compensated in the reconstructed images by arc correction.

## **Images at the Scanner Centre**

**Figure 3** shows the central plane reconstructed image from the Jaszczak SPECT phantom mounted at the centre of the field of view, with and without attenuation correction. The phantom contains 6 sets of cold rods, of which the largest (12.7 mm diameter) rods are clearly visible, as are the second set (11.1 mm). The third set of rods (9.5 mm) is also just visible in the attenuation corrected image. This image corresponds to a total of 45M events (all 15 planes).



**Figure 2.** Sinograms produced by imaging the Jaszczak SPECT phantom at different locations in the scanner field of view. (a) At the centre; (b) At 25 cm off centre; (c) At 45 cm off centre.



**Figure 3.** Image of the central Jaszczak SPECT phantom. (a) Without attenuation correction and (b) With attenuation correction.

### 3.2. Uniform Phantom

Two types of uniform cylindrical phantom containing short (18-F) and long half life (68-Ge) sources were used for investigating the uniformity and noise level of the reconstructed images.

#### 3.2.1. Short Half Life Uniform Phantom

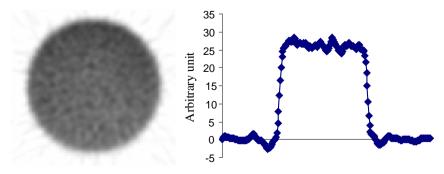
The short half life uniform phantom was prepared from a 20 cm diameter cylindrical phantom with an axial length of 20 cm filled with 18-F solution only to the depth of the FOV. **Figure 4** shows image plane from the 20 cm diameter uniform phantom, positioned at the centre of the field of view, imaged at the value of specific activity: 100 M counts in 600 s. Also shown in each case is the horizontal profile across the image. The coefficient of Variation (CV) of the image was calculated as  $5.7\% \pm 0.2\%$  from the ratio of standard deviation ( $\sigma$ ) to the mean pixel counts ( $\mu$ ). Some of the other image planes show weak ring artefacts in the reconstructed images. The source of these artefacts and variations needs to be further investigation.

## 3.2.2. Long Half Life Uniform Phantom

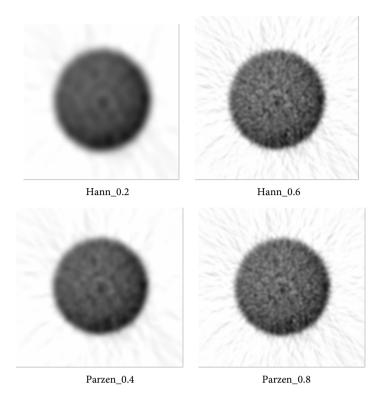
Reconstructed images of a central slice (slice 8) of the phantom using Hann filter with cutoff frequency of 0.2 and 0.6, and the same plane reconstructed by Parsen filter with cutoff frequency of 0.4 and 0.8 are shown in **Figure 5**. The image (top-left) with low cut-off frequency shows ringing artefact and the image (bot-tom-left) shows a similar artefact, but suppress the noise. Conversely, the images (top- and bottom-right) with higher cut-off frequency do not show any artefact, but introduce noise.

The coefficient of variation for a central slice of the uniform cylindrical source versus the filter cutoff frequency for three filters (Hann, Hamming and Parzen) is shown in **Figure 6**. The values of CV for Parzen filter are lower than the values for Hann and Hamming filters. The CV results for Hann and Hamming filters are very similar (slightly higher in case of Hamming filter) and are increasing approximately in linear fashion with the increase of cutoff frequency. The CV results in **Figure 6** are consistent with the images in **Figure 5** and are also consistent with other study [7] using mini PET [8].

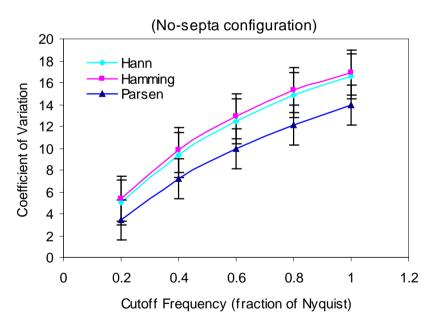
The coefficient of variation for all image planes of the same phantom were al-



**Figure 4.** Uniform phantom image and the corresponding horizontal profile across the centre of the image.

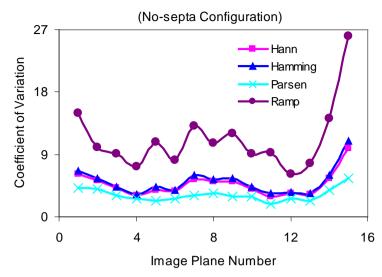


**Figure 5.** Image plane (plane 8) for a uniform 68-Ge cylindrical phantom recon structed with Hann and Parzen filter and its different cut-off frequency.



**Figure 6.** Coefficient of variation  $(\sigma l \mu)$  for a central plane (plane 8) of a 68-Ge uniform cylinder as a function of cutoff frequency for three filters.

so computed for different filters using a cutoff frequency of 0.2 as shown in Figure 7. The Parsen filter consistently gives lower CV values than the other filters and also gives less variation in CV between planes. The Hann and Hamming filters give indistinguishable results for all planes. In all cases planes 4 - 6 and 11 - 13 have lower CV values than the other planes.



**Figure 7.** Coefficient of Variation ( $\sigma \mu$ ) for a 68-Ge uniform cylinder as a function of image plane number for different filters.

### 4. Conclusion

The Jaszczak SPECT phantom contains 6 sets of cold rods, of which the largest (12.7 mm diameter) rods are clearly visible, as are the second set (11.1 mm). The third set of rods (9.5 mm) is also just visible in the attenuation corrected image. For uniform phantom images, the coefficient of variation increases with cutoff frequency as expected. All filters with low cut off-frequency (<0.6) would suppress image noise but decrease contrast. The value of CV for the Parsen filter is lower than the value for Hann and Hamming filters.

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