

The Impact of Variation in Bladder Volume on the **Doses of Target and Organ-at-Risk in Intensity-Modulated Radiation Therapy for Localized Prostate Cancer**

Shogo Hatanaka^{1*}, Yoshito Kawada¹, Kana Washizu¹, Nobuko Utsumi^{1,2}, Takafumi Yamano¹, Keiichiro Nishimura¹, Tetsuya Watanabe¹, Katsuhito Hosaka¹, Keisuke Todoroki¹, Go Nakajima¹, Munefumi Shimbo¹, Takeo Takahashi¹

¹Department of Radiation Oncology, Saitama Medical Center, Saitama Medical University, Kawagoe City, Japan ²Department of Radiology, JCHO Tokyo Shinjuku Medical Center, Tokyo, Japan

Email: *hatasho@saitama-med.ac.jp

How to cite this paper: Hatanaka, S., Kawada, Y., Washizu, K., Utsumi, N., Yamano, T., Nishimura, K., Watanabe, T., Hosaka, K., Todoroki, K., Nakajima, G., Shimbo, M. and Takahashi, T. (2016) The Impact of Variation in Bladder Volume on the Doses of Target and Organ-at-Risk in Intensity-Modulated Radiation Therapy for Localized Prostate Cancer. Journal of Cancer Therapy, **7**, 741-751.

http://dx.doi.org/10.4236/jct.2016.710075

Received: September 13, 2016 Accepted: October 4, 2016 Published: October 7, 2016

Copyright © 2016 by authors and Scientific Research Publishing Inc. This work is licensed under the Creative **Commons Attribution International** License (CC BY 4.0).

http://creativecommons.org/licenses/by/4.0/ **Open Access**

۲

Abstract

Intensity-modulated radiation therapy (IMRT) has become the mainstay of treatment for localized prostate cancer. In IMRT, minimizing differences between the conditions used during planning CT and daily treatment is important to prevent adverse events in normal tissues. In the present study, we evaluated the impact of variation in bladder volume on the doses to various organs. A total of 35 patients underwent definitive radiotherapy at Saitama Medical Center. A Light Speed RT16 (GE Healthcare) was used for planning and to obtain examination CT images. Such images were acquired after 4 - 6 days of planning CT image acquisition. The IMRT plans were optimized using the planning CT data to satisfy the dose constraints set by our in-house protocols for the PTV and the OARs. The dose distributions were then re-calculated using the same IMRT beams, and checked on examination CT images. It was clear that bladder volume affected the doses to certain organs. We focused on the prostate, bladder, rectum, small bowel, and large bowel. Regression coefficients were calculated for variables that correlated strongly with bladder volume (p < 0.05). We found that variation in bladder volume [cm³] predicted deviations in the bladder V_{70Gy} , V_{50Gy} , and V_{30Gy} [%]; the maximum dose to the small bowel [cGy]; and the maximum dose to the large bowel [cGy]. The regression coefficients were -0.065, -0.125, -0.180, -10.22, and -9.831, respectively. We evaluated the impacts of such variation on organ doses. These may be helpful when checking a patient's bladder volume before daily IMRT for localized prostate cancer.

Keywords

Bladder Volume, Localized Prostate Cancer, Intensity-Modulated Radiation Therapy, Dose to Organs at Risk, Computed Tomography

1. Introduction

Prostate cancer is the most common cancer in men, and intensity-modulated radiation therapy (IMRT) has become the mainstay of treatment for localized prostate cancer. IMRT delivers radiation more precisely than earlier techniques, sparing surrounding normal tissue [1]. In IMRT, an inverse planning technique is used to optimize the dose distribution. Such optimization is performed with the aid of computed tomography (CT) images. However, daily variations in organ conditions are not considered when calculating the doses delivered to organs at risk (OARs). Therefore, minimizing the differences between organ conditions during planning CT and those during daily treatment is important to prevent adverse events in normal tissues.

In the present study, we evaluated the impact of variation in bladder volume (the amount of urine) on the target and OAR doses during localized prostate IMRT. One possible advantage of maintaining a full bladder is that part of the bladder moves away from the target volume, thereby reducing bladder toxicity [2] [3]. A full bladder also moves the small and large bowels out of the irradiation field, reducing toxicity to these organs [4]-[8]. However, if large bladder volumes are used during CT planning and radiotherapy, such volumes tend to exhibit marked variability [9]-[11]. Thus, a bladder volume of about 150 cm³ is more suitable for planning [12], and it is important to confirm that the bladder volume during daily treatment is the same.

Transabdominal bladder ultrasound devices and in-room CT techniques (e.g., kV Cone-beam CT, MV Cone-beam CT, and On-rail CT) can be used to measure bladder volume [2]-[14]. In-room CT increases the doses to normal tissues. In contrast, ultrasound techniques are non-invasive, rapid, and inexpensive [9] [10] [13]; they are thus useful when checking the bladder volume in patients undergoing localized prostate IMRT. Given the time constraints of clinical practice, it is difficult to perfectly equalize the bladder volume during radiotherapy to that during planning CT. Criteria for determining whether to take any action, such as extending the urine collection time, are required. However, no previous report has focused on the impact of bladder volume variation on target and OAR doses during IMRT for localized prostate cancer. We therefore addressed the topic.

2. Methods and Materials

2.1. Patients and CT Image Acquisition

Between June 2015 and May 2016, 35 patients underwent definitive radiotherapy at Saitama Medical Center. All procedures used in this research were approved by the Ethical Committee of Saitama Medical Center. **Table 1** shows the patient characteristics. The patients were irradiated in a supine position with the aid of a thermoplastic seat (**Figure 1**). A Light Speed RT16 (GE Healthcare, Little Chalfont, UK) was used for planning CT and acquisition of the examination CT images used to determine the reproducibility of organ conditions (4 - 6 days after planning CT image acquisition). Body surface markers placed at the time of planning CT image acquisition were used to align the CT images (2.5 mm in slice thickness). Patients were instructed to drink a fixed volume of water 30 - 60 min before CT image acquisition; urination was prohibited to enable appropriate acquisition. The CT images were examined for rectal gas by a radiation oncologist. If necessary, additional CT images were acquired based on the recommendation that the diameter of the rectum, measured transversely at the base, should be >4 cm [15]. Cone-Beam CT images have been used for evaluation of the



Figure 1. The thermoplastic seat used to immobilize the patients.

		Data
Age	Median	78
	Range	53 - 84
Clinical stage	T1	6
	T2	15
	T3	12
	T4	2
PSA	Mean	29.8
	Range	4.3 - 220.9
Gleason score	≤7	12
	8	14
	≥9	9

variations in organ conditions in several reports [14] [16]. However, the dose calculation using Cone-Beam CT images are required the CT values corrections [17]-[19], so the uncertainty of the dose calculation using Cone-Beam CT images is greater than that using Fan-Beam CT images. Additionally, Fan-Beam CT image qualities are higher than Cone-Beam CT image qualities. Thus, Fan-Beam CT images were used for evaluation in this study.

2.2. Contours

XiO version 5.00 (Elekta, Stockholm, Sweden) was the Radiation Treatment Planning System (RTPS) used. Target and organ volumes were determined, based on the planning CT images, by a radiation oncologist and a medical physicist. **Figure 2** shows the example of target and organ volumes determined in this study. A prostate clinical target volume (CTV) and planning target volume (PTV) were defined. The CTV was the prostate with 10 mm of the proximal seminal vesicle. All seminal vesicles were included in the CTV (in cases of clinical T3b stage disease). PTV was defined as the CTV plus a 10 mm margin (rectal side: 5 mm). The OARs were the rectum (from the ischial tuberosities to the rectosigmoid flexure), the rectal wall within 10 mm above and below the PTV (wall thickness: 4 mm), the bladder, the bladder wall (wall thickness: 4 mm), and the small and large bowels. The bladder volume was calculated using the planning CT images.

2.3. Planning

The linac model of Clinac 21EX (Varian Medical Systems, Palo Alto, CA; X-ray energy: 10 MV) was used for planning. Step-and-shoot IMRT plans were created based on the planning CT images using seven coplanar photon beams (gantry angles: 0°, 50°, 100°, 145°, 215°, 260°, and 310°). The prescribed dose to 95% of the PTV was 74 Gy in 37 fractions. The dose calculation grid size was always set to 2 mm. The iso-center was the center of the prostate. Superposition [20] [21], with heterogeneous correction, was used as the dose calculation algorithm.

Table 2 shows the dose constraints employed. The treatment plans were optimized to satisfy constraints defined by our in-house protocols for doses to the PTV and OARs.

2.4. Re-Calculation Using Examination CT Images

Target and organ volumes were determined, based on the examination CT images, by a radiation oncologist and a medical physicist. The bladder volumes on the examination CT images, and the relative variations in such volumes between the planning and examination CT images, were calculated using the formula below. V_{b-c} is the bladder volume on examination CT and V_{b-p} the bladder volume on planning CT (for the same patient). Dose distributions were then re-calculated using the examination CT images and the same IMRT beams described above. The iso-center was set at the coordinates indicated by planning CT.

Bladder volume variation $\left\lceil \text{cm}^3 \right\rceil = V_{b-c} - V_{b-p}$



Figure 2. The example of target and organ volumes determined in this study.

Table 2. Dose constraints used in this study.

Contour	Index	Optimal
	D _{95%} [Gy]	>74
	Mean dose [Gy]	73.26 - 76.22
PIV	D _{max} [Gy]	<79.18
	$V_{98\%}$ [%]	>98
	V _{65Gy} [%]	<17
Rectum	V _{40Gy} [%]	<35
	V _{20Gy} [%]	<60
Rectal wall	V _{78Gy} [%]	<1
	V _{70Gy} [%]	<20
	V _{60Gy} [%]	<30
	V _{40Gy} [%]	<60
Bladder	V _{54Gy} [%]	<25
	V _{33Gy} [%]	<50
Dia 1 dae 11	V _{70Gy} [%]	<35
Bladder wall	V _{40Gy} [%]	<60
Small bowel	$V_{60{ m Gy}}[{ m cm}^3]$	<0.5
Large bowel	$V_{65Gy} [{ m cm}^3]$	<0.5

2.5. Evaluation of the Target Volume Dose

The coordinates of the center of the prostate (left-right, superior-inferior, and anterior-posterior) and those of the CTV doses ($D_{98\%}$ and $V_{90\%}$) were compared between the planning and examination CT images, and deviations calculated using the RTPS. The impacts of bladder volume variation on prostate position and CTV dose were explored. Pearson correlation coefficients (*r*) with *p*-values were calculated. A difference was considered significant if the two-tailed p-value was <0.05. SPSS version 23 software (IBM Corp., Armonk, NY) was used for statistical analysis.

2.6. Evaluation of the Doses to OARs

The doses to the bladder (maximum dose $[D_{max}]$, V_{70Gy} , V_{50Gy} , and V_{30Gy}), bladder wall (D_{max} , V_{70Gy} , V_{50Gy} , V_{50Gy} , and V_{30Gy}), rectum (D_{max} , V_{70Gy} , V_{50Gy} , and V_{30Gy}), rectal wall (D_{max} , V_{70Gy} , V_{50Gy} , and V_{30Gy}), and the small and large bowel (D_{max} values) were calculated using the RTPS; deviations were also calculated using the RTPS. The impact of bladder volume variation on doses to the OARs was explored. Pearson correlation coefficients (r) with p-values were calculated. A difference was considered significant if the two-tailed p-value was <0.05. SPSS version 23 software (IBM Corp.) was used for statistical analysis.

2.7. Linear Regression

We subjected variables that correlated strongly with bladder volume (p < 0.05) to a regression analysis and calculated regression coefficients with 95% confidence intervals (CIs). SPSS version 23 software (IBM Corp.) was used for statistical analysis.

3. Results

The mean bladder volume (± 1 standard deviation) was 191 mL (± 93 mL) on planning CT and 148 mL (± 81 mL) on examination CT.

Table 3 shows the outcomes of a univariate analysis of associations with variation in bladder volume. Such variation predicted deviations in the bladder V_{30Gy} - V_{70Gy} , the bladder wall V_{30Gy} - V_{70Gy} , and the small and large bowel D_{max} values. In contrast, variation in bladder volume did not predict deviations in the doses to the prostate or the CTV, the bladder D_{max} , the bladder wall D_{max} , or the rectum or rectal wall doses.

Table 4 lists the regression coefficients between bladder volume variation and each dependent variable. **Figure 3** shows the deviations in the bladder and the bladder wall V_{70Gy} , V_{50Gy} , and V_{30Gy} as functions of bladder volume variation. The regression coefficients (with 95% CIs) were -0.065 (-0.088 to -0.042), -0.125 (-0.154 to -0.096), -0.180 (-0.211 to -0.149), -0.054 (-0.069 to -0.038), -0.099 (-0.121 to -0.078), and -0.152 (-0.178 to -0.125), respectively. **Figure 4** shows the deviations in the small and large bowel D_{max} values as functions of bladder volume variation. The regression coefficients (with 95% CIs) were -10.22 (-15.69 to -4.743) and -9.831 (-13.96 to -5.702), respectively. Thus, a smaller bladder increased the dose to the OARs.

4. Discussion

The mean bladder volume during planning CT was larger than that during examination CT. Creation of a thermoplastic seat and body surface marking were required for planning CT, so the patient set-up time was longer than for examination CT. We did not engage in detailed verification; however, the observed difference in bladder volume may be attributable to the longer patient set-up time for planning CT.

Variable		r	p		
Coordinates of the	L-R [cm]	0.034			
Coordinates of the	S-I [cm]	-0.076	N.S.		
prostate center	A-P [cm]	-0.045			
CTV	$D_{98\%}$ [Gy]	-0.067	NC		
	V _{90%} [%]	-0.018	N.5.		
	D _{max} [Gy]	0.005	N.S.		
Bladder	V _{70Gy} [%]	-0.775	< 0.01		
	V _{50Gy} [%]	-0.861	< 0.01		
	V _{30Gy} [%]	-0.910	< 0.01		
Bladder wall	D _{max} [Gy]	-0.050	N.S.		
	V _{70Gy} [%]	-0.810	< 0.01		
	$V_{50Gy}[\%]$	-0.868	< 0.01		
	V _{30Gy} [%]	-0.902	< 0.01		
	D _{max} [Gy]	0.019			
Rectum	V _{70Gy} [%]	0.115			
	V _{50Gy} [%]	0.036	N.S.		
	V _{30Gy} [%]	-0.018			
Rectal wall	D _{max} [Gy]	-0.027			
	V _{70Gy} [%]	0.012	NLC.		
	V _{50Gy} [%]	-0.027	N.5.		
	V _{30Gy} [%]	-0.011			
Small bowel	D _{max} [cGy]	-0.629	<0.01		
Large bowel	D _{max} [cGy]	-0.641	<0.01		

Table 3. Univariate analysis of associations with variation in bladder volume [cm³].

*L-R: left-right; S-I: superior-inferior; A-P: anterior-posterior; N.S.: not significant.

Table 4.	Regression	coefficients	between	bladder	volume	variation	$[cm^3]$	and	the	depende	nt
variables.											

OAR	Index	Regression coefficient (95% CI)
	V _{70Gy} [%]	-0.065 (-0.088, -0.042)
Bladder	V _{50Gy} [%]	-0.125 (-0.154, -0.096)
	V _{30Gy} [%]	-0.180 (-0.211, -0.149)
	V _{70Gy} [%]	-0.054 (-0.069, -0.038)
Bladder wall	V _{50Gy} [%]	-0.099 (-0.121, -0.078)
	V _{30Gy} [%]	-0.152 (-0.178, -0.125)
Small bowel	D _{max} [cGy]	-10.22 (-15.69, -4.743)
Large bowel	D _{max} [cGy]	-9.831 (-13.96, -5.702)

We did not find a significant association between prostate position and variation in bladder volume. Similarly, we found no significant association between the dose to the CTV and bladder volume variation. Therefore, if the chosen margin allows for inter-fractional errors in other factors (e.g., set-up error), the impacts of bladder volume variation on target position and dose may be negligible.



Figure 3. The relationship between variation in bladder volume and deviation in bladder dose (Left: Bladder; Right: Bladder wall).



Figure 4. The relationship between variation in bladder volume and deviations in the small and large bowel D_{max} values.

For the rectum and rectal wall, we found no significant association between the D_{max} and $V_{30\text{Gy}}$ - $V_{70\text{Gy}}$ and bladder volume deviation. Thus, the impact of such variation on the rectal dose may be negligible.

For the bladder and bladder wall, we found no significant association between the D_{max} values and bladder volume variation. As part of the bladder overlapped with the PTV in all cases, the bladder D_{max} and the dose to the internal region of the PTV were approximately equal. Additionally, the treatment plans were optimized to render the internal PTV dose uniform. Therefore, the bladder D_{max} was not significantly affected by bladder volume variation. On the other hand, we did find significant associations between the bladder and bladder wall $V_{30\text{Gy}}$ - $V_{70\text{Gy}}$ values and bladder volume variation. The smaller the bladder, the greater the proportion of the bladder that lies near the tar-

get volume. Therefore, a reduction in bladder volume increases the bladder dose, and it is thus important to check that the bladder volume during daily treatment is greater than that during planning CT.

For both the small and large bowel, we found significant associations between the D_{max} values and bladder volume variation. A smaller bladder moves the small and large bowel near the irradiation field [4]-[8] and increases the doses to these organs. A previous report showed that TD 50/5 of small bowel was 60 Gy (for 1/3 of the volume) and TD 50/5 of large bowel was 65 Gy (for 1/3 of the volume) [2]. It is thus important to check that the bladder volume during daily treatment is greater than that during planning CT. Additionally, it is also important to check that the doses of small and large bowel are <60 Gy and 65 Gy, respectively. If the amount of urine is inadequate, an extension of time to allow urine to collect in the bladder should be considered to reduce the doses to these organs. The criteria whether the amount of urine is adequate can be decided by using the bladder volume and the doses to the OARs during planning CT, the dose constraints, and the regression coefficients in this study.

No previous report has quantitatively evaluated the effects of bladder volume variation on organ doses during IMRT for localized prostate cancer. We found that variation in bladder volume predicted deviations in the bladder V_{30Gy} - V_{70Gy} , bladder wall V_{30Gy} - V_{70Gy} , and small and large bowel D_{max} values. The absence of a bladder volume check may increase the doses to OARs. An ultrasound device can be used to measure bladder volume non-invasively, rapidly, and inexpensively [9] [10] [13]. Such a device should be used to check the bladder volume prior to daily localized prostate IMRT; this is very important. Our results may be useful when choosing an appropriate bladder volume for each patient.

5. Conclusion

We evaluated the effect of bladder volume variation on organ doses, and we developed bladder volume criteria. Our results may be useful when checking the bladder volume before daily IMRT for patients with localized prostate cancer.

Acknowledgements

This work was partly supported by a Kanto-Branch Research Grant from the Japanese Society of Radiological Technology.

References

- Pizkall, A., Carol, M., Lohr, F., *et al.* (2000) Comparison of Intensity-Modulated Radiotherapy with Conventional Conformal Radiotherapy for Complex-Shaped Tumors. *International Journal of Radiation Oncology * Biology * Physics*, 48, 1371-1380. http://dx.doi.org/10.1016/S0360-3016(00)00772-0
- [2] Emami, B., Lyman, J., Brown, A., et al. (1991) Tolerance of Normal Tissue to Therapeutic Irradiation. International Journal of Radiation Oncology * Biology * Physics, 21, 109-122. http://dx.doi.org/10.1016/0360-3016(91)90171-Y
- [3] Marks, L.B., Carroll, P.R., Dugan, T.C., et al. (1995) The Response of the Urinary Bladder,

Urethra, and Ureter to Radiation and Chemotherapy. International Journal of Radiation Oncology * Biology * Physics, 31, 1257-1280. http://dx.doi.org/10.1016/0360-3016(94)00431-J

- [4] De Meerleer, G.O., Villeirs, G.M., Vakaet, L., et al. (2004) The Incidence of Inclusion of the Sigmoid Colon and Small Bowel in the Planning Target Volume in Radiotherapy for Prostate Cancer. Strahlentherapie und Onkologie, 180, 573-581. http://dx.doi.org/10.1007/s00066-004-1267-5
- [5] Brierley, J.D., Cummings, B.J., Wong, C.S., et al. (1994) The Variation of Small Bowel Volume within the Pelvis before and during Adjuvant Radiation for Rectal Cancer. Radiotherapy and Oncology, 31, 110-116. http://dx.doi.org/10.1016/0167-8140(94)90390-5
- [6] Kim, T.H., Chie, E.K., Kim, D.Y., et al. (2005) Comparison of the Belly Board Device Method and the Distended Bladder Method for Reducing Irradiated Small Bowel Volumes in Preoperative Radiotherapy of Rectal Cancer Patients. International Journal of Radiation Oncology * Biology * Physics, 62, 769-775. http://dx.doi.org/10.1016/j.ijrobp.2004.11.015
- [7] Muren, L.P., Smaaland, R. and Dahl, O. (2003) Organ Motion, Set-Up Variation and Treatment Margins in Radical Radiotherapy of Urinary Bladder Cancer. Radiotherapy and Oncology, 69, 291-304. http://dx.doi.org/10.1016/S0167-8140(03)00246-9
- [8] Waldenström, A.C., Alsadius, D., Pettersson, N., et al. (2010) Variation in Position and Volume of Organs at Risk in the Small Pelvis. Acta Oncologica, 49, 491-499. http://dx.doi.org/10.3109/02841861003702536
- [9] Stam, M.R., van Lin, E.N., van der Vight, L.P., et al. (2006) Bladder Filling Variation during Radiation Treatment of Prostate Cancer: Can the Use of a Bladder Ultrasound Scanner and Biofeedback Optimize Bladder Filling? International Journal of Radiation Oncology * Biology * Physics, 65, 371-377.
- [10] O'Doherty, U.M., McNair, H.A., Norman, A.R., et al. (2006) Variability of Bladder Filling in Patients Receiving Radical Radiotherapy to the Prostate. Radiotherapy and Oncology, 79, 335-340. http://dx.doi.org/10.1016/j.radonc.2006.05.007
- [11] Nakamura, N., Shikama, N., Takahashi, O., et al. (2010) Variability in Bladder Volumes of Full Bladders in Definitive Radiotherapy for Cases of Localized Prostate Cancer. Strahlentherapie und Onkologie, 186, 637-642. http://dx.doi.org/10.1007/s00066-010-2105-6
- [12] Nakamura, N., Shikama, N., Takahashi, O., et al. (2012) The Relationship between the Bladder Volume and Optimal Treatment Planning in Definitive Radiotherapy for Localized Prostate Cancer. Acta Oncologica, 51, 730-734. http://dx.doi.org/10.3109/0284186X.2011.639388
- [13] Hynds, S., McGarry, C.K., Mitchell, D.M., et al. (2011) Assessing the Daily Consistency of Bladder Filling Using an Ultrasonic Bladderscan Device in Men Receiving Radical Conformal Radiotherapy for Prostate Cancer. The British Journal of Radiology, 84, 813-818. http://dx.doi.org/10.1259/bjr/50048151
- [14] Hirose, Y., Nakamura, M., Tomita, T., et al. (2014) Evaluation of Different Set-Up Error Corrections on Dose-Volume Metrics in Prostate IMRT Using CBCT Images. Journal of Radiation Research, 55, 966-975. http://dx.doi.org/10.1093/jrr/rru033
- [15] deCrevoisier, R., Tucker, S.L., Dong, L., et al. (2005) Increased Risk of Biochemical and Local Failure in Patients with Distended Rectum on the Planning CT for Prostate Cancer Radiotherapy. International Journal of Radiation Oncology * Biology * Physics, 62, 965-973. http://dx.doi.org/10.1016/j.ijrobp.2004.11.032
- [16] Sripadam, R., Stratford, J., Henry, A.M., Andrew, J., Moore, C.J. and Price, P. (2009) Rectal Motion Can Reduce CTV Coverage and Increase Rectal Dose during Prostate Radiothera-



py: A Daily Cone-Beam CT Study. *Radiotherapy and Oncology*, **90**, 312-317. http://dx.doi.org/10.1016/j.radonc.2008.07.031

- [17] Guan, H. and Dong, H. (2009) Dose Calculation Accuracy Using Cone-Beam CT (CBCT) for Pelvic Adaptive Radiotherapy. *Physics in Medicine and Biology*, 54, 6239-6250. <u>http://dx.doi.org/10.1088/0031-9155/54/20/013</u>
- [18] Rong, Y., Smilowitz, J., Tewatia, D., Tomé, W.A. and Paliwal, B. (2010) Dose Calculation on kV Cone Beam CT Images: An Investigation of the Hu-Density Conversion Stability and Dose Accuracy Using the Site-Specific Calibration. *Medical Dosimetry*, **35**, 195-207. http://dx.doi.org/10.1016/j.meddos.2009.06.001
- [19] Hu, W., Ye, J., Wang, J., Ma, X. and Zhang, Z. (2010) Use of Kilovoltage X-Ray Volume Imaging in Patient Dose Calculation for Head-And-Neck and Partial Brain Radiation Therapy. *Radiation Oncology*, 5, 29. <u>http://dx.doi.org/10.1186/1748-717X-5-29</u>
- [20] Miften, M., Wiesmeyer, M., Monthofer, S. and Krippner, K. (2000) Implementation of FFT Convolution and Multigrid Superposition Models in the FOCUS RTP System. *Physics in Medicine and Biology*, 45, 817-833. <u>http://dx.doi.org/10.1088/0031-9155/45/4/301</u>
- [21] Miften, M., Wiesmeyer, M., Kapur, A. and Ma, C.M. (2001) Comparison of RTP Dose Distributions in Heterogeneous Phantoms with the BEAM Monte Carlo Simulation System. *Journal of Applied Clinical Medical Physics*, 2, 21-31.

Scientific Research Publishing

Submit or recommend next manuscript to SCIRP and we will provide best service for you:

Accepting pre-submission inquiries through Email, Facebook, LinkedIn, Twitter, etc. A wide selection of journals (inclusive of 9 subjects, more than 200 journals) Providing 24-hour high-quality service User-friendly online submission system Fair and swift peer-review system Efficient typesetting and proofreading procedure Display of the result of downloads and visits, as well as the number of cited articles Maximum dissemination of your research work Submit your manuscript at: <u>http://papersubmission.scirp.org/</u>

Or contact jct@scirp.org