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The Influences of an Embedded Structure Fiber-Optic Radiation Dosimeter in Different SSD and Beam Field Size

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Abstract

With a rapidly increasing demand and widespread use of radiotherapy treatment, the subject area of *in-vivo* real time dose rate dosimeters has become a significant area of study. An embedded structure fiber-optic radiation dosimeter has proved to be a promising candidate to fulfil this role because of its high SNR (signal-to-noise ratio) and excellent light conversion efficiency. In this paper, the properties of this kind of dosimeter with respect to different SSD (Source to Surface Distance) and beam field size in a clinical Linac are studied. The characteristics of the dosimeter were evaluated by the sensor's output intensity response in these conditions.

Keywords

Optical Fiber Sensing, Radiation, SSD (Source to Surface Distance), Beam Field Size

1. Introduction

In-vivo radiation dosimeters have become a promising research direction in recent years because of their ability of real-time measurement. They have the advantage of allowing intervention in time if a potential accidental over or under dose is monitored during radiotherapy [1]. In this condition, a series of dosimeters have carried out such as TLDs, optic fiber coupled organic scintillators and

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doped silica glass. The general use of optic fiber as sensing section has become increasingly widely used in dosimetry field. For example, Beddar *et al.* developed a "scintillator-fiber optic-PMT" detector which made optical fiber coupled to the miniature organic scintillator [2]. This kind of detector can satisfy the requirement for water-equivalence and linearity with dose and energy independence in the megavoltage (photon) energy range. However, it has lower sensitivity and some organic scintillators also exhibit the disadvantage of being temperature dependent [3]. These factors represent a significant barrier to practical application. Issa *et al.* proposed Ge-doped silica fibers for use in *in-vivo* brachytherapy applications [4]. This detector is based on TL technology. Therefore, a significant drawback to this technique is that owing to the requirement to stimulate the material to produce a signal sometime after irradiation, it cannot deliver real-time dosimetry [5].

To overcome these disadvantages mentioned above, Qin *et al.* and O'Keeffe *et al.* developed a method of inserting inorganic scintillator inside the core of PMMA fibers called embedded structure fiber-optic radiation dosimeter , it can achieve a high SNR and excellent light conversion efficiency [6] [7]. And this dosimeter has been proved to have the properties of excellent repeatability, being isotropic and linearity in the condition of the beam field size of $10 \times 10 \text{ cm}^2$ at a SSD (Source to Surface Distance) of 100 cm. In this paper, the intensity response of this dosimeter in different SSD and beam field size was investigated.

2. Methodology

The dosimeter used in this paper consists of a 25 m long PMMA fiber (0.5 mm diameter) (ESKA SH2001-J) with an inorganic scintillator, Gd_2O_2S : Tb (terbium-doped gadolinium oxysulfide) embedded in the core of the fiber. The schematic representation and graph of the detector probes for this dosimeter is shown in **Figure 1**.

The scheme of the experiment is shown in **Figure 2**. The dosimeter is placed inside a standard water tank which can also accommodate an Ionization Chamber (IC) for reference measurement of dose. When the probe of the dosimeter is irradiated using the X-Ray from the Linac, the scintillator inside the PMMA fiber emits visible light which is transmitted through the 25 m length of fiber and

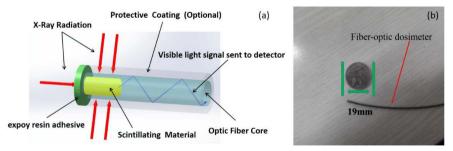


Figure 1. The embedded structure fiber-optic radiation dosimeter (a) schematic representation (b) photograph.

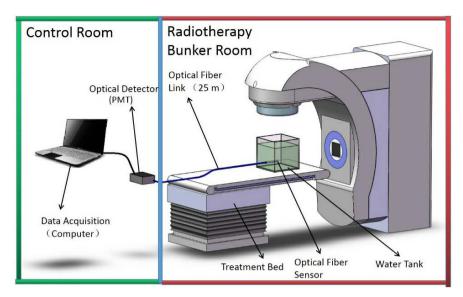


Figure 2. The device scheme of the experiment.

finally detected using a Photomultiplier Tube (PMT) (Hamamatsu PMT CH-253).

3. Results and Discussion

3.1. The Intensity Response of the Dosimeter in Different SSD

The intensity response of the IC and optical fiber dosimeter with different SSD is shown in **Figure 3**. Both the IC and optical fiber dosimeter were placed in the water tank at the depth of 1.5 cm as this depth is the D_{max} in water. This experiment was performed for a dose rate of 600 MU/min for the full beam pulse time of 20 s. The beam photon energy used in this experiment was 6 MV.

Figure 3 shows that both the IC and optical fiber dosimeter's intensity response follow the square inverse law. The fitting equations of them can be expressed as follow:

$$y = 10.7281 + 3775062.0115x^{-2}$$
 (1)

$$y = 5058 + 1.205 \times 10^8 \, x^{-2} \tag{2}$$

For which (1) corresponds to the IC and (2) to the optical fiber dosimeter. The error of the measured values and calculated values (obtained from Equation (1) and (2)) of IC and optical fiber dosimeter is shown in **Table 1**.

From **Table 1**, it can be seen that both IC and the dosimeter follow the fitting equation well, the error of the measured and calculated value being less than 1.5%. Therefore, the results verify that the optical fiber dosimeter (and IC) obey the inverse square law.

As both IC and the optical fiber dosimeter follow the inverse square law, the relationship of the dosimeter and IC for the same range of SSD values is shown in **Figure 4** (The red curve is the fitting curve).

The result of Figure 4 demonstrate that the dosimeter and IC have a strong

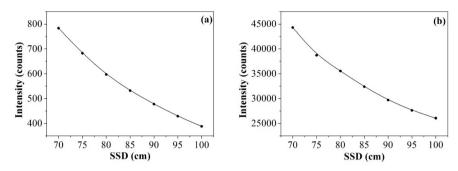


Figure 3. Intensity response in different SSD (a) IC; (b) dosimeter.

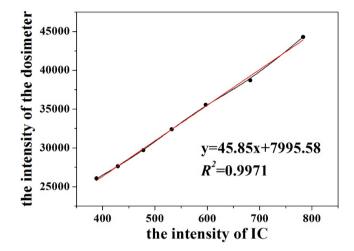


Figure 4. The relationship of the dosimeter and IC in same SSD.

Table 1. The real and calculated intensity output of IC and dosimeter in different SSD.

SSD (cm)	IC			Dosimeter		
	Measured value	Calculated value	Error (100%)	Measured value	Calculated value	Error (100%)
70	783.2	781.14	0.26	44,285.1	43,830.16	1.03
75	682.2	681.84	0.05	38,701	39,266.44	-1.46
80	597	600.57	-0.60	35,551.4	35,531.38	0.06
85	532	533.22	-0.23	32,396.1	32,435.84	-0.12
60	477.7	476.78	0.19	29,702.5	29,841.75	-0.47
65	429.2	429.01	0.04	27,616.3	27,646.38	-0.11
100	388.3	388.23	0.02	26,060.1	25,772	1.11

linear relationship over the range of SSD tested. A linear regression analysis of the data of **Figure 4** indicates an R^2 value of 0.9971, and hence if the output intensity for a certain SSD is obtained, it is possible that the absorbed dose can be accurately determined.

3.2. The Intensity Response of the Dosimeter in Different Beam Field Size

Previous studies of the embedded structure fiber-optic radiation dosimeter have usually focused on the exposure condition with the standard beam field size of 10×10 cm² [7] [8]. It is also meaningful to establish the response of the optical fiber dosimeter to different beam size. The dosimeter was exposed in beam field sizes of 3×3 cm², 4×4 cm², 5×5 cm², 6×6 cm², 7×7 cm², 8×8 cm², 9×9 cm², 10×10 cm², 15×15 cm², 20×20 cm², 25×25 cm² and 30×30 cm² at the water depth of 1.5 cm (D_{max}) and SSD of 100 cm. The beam electron energy used in this experiment was 6 MeV. The intensity output response is shown in **Figure 5**.

Figure 5 shows that the intensity output response of the dosimeter initially increases as the area of beam field sizes get larger. The rate of increase is initially highest when the beam field size within 10×10 cm² and then becomes slower and is finally invariant above 20×20 cm². When the beam field size is less than 10×10 cm², the relationship of the beam field size and output intensity closely obeys linearity (R^2 of 0.996).

4. Conclusion

An investigation has been carried out to study the characteristics of an embedded structure fiber-optic radiation dosimeter with different SSD and beam field size. The experiment results indicated that the dosimeter closely obeys the inverse square law in the SSD range tested (70 - 100 cm) and the relationship of the simultaneously measure dose using an IC and the optical fiber dosimeter is strongly linear (R^2 of 0.9971). This phenomenon shows that it may be possible to retrieve the absorbed dose information when SSD is known. The intensity response of the dosimeter for different beam field sizes was also investigated. And the response is a curve who's initial region (0 to $10 \times 10 \text{ cm}^2$) linearly (R^2 of 0.996) but which reaches saturation (Becoming invariant with beam size above a value of $20 \times 20 \text{ cm}^2$).

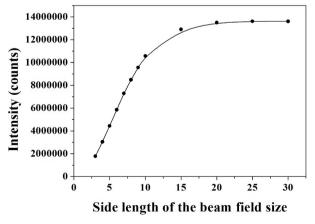


Figure 5. The intensity output response of the dosimeter in different beam field size.

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