Exploring the useful exposure range limits of three intraoral image receptors for various tube potential, tube current and exposure time settings

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ABSTRACT

Objectives: To determine the useful exposure range limits of three intraoral image receptors of different technology when exposed to different X-ray beam spectra, dose and dose rate levels. Study Design: A dental X-ray unit offering a wide range of tube potential, tube current and exposure time settings was used to expose a dental quality control phantom. The receptors that were used to capture the radiographic images of the phantom were: the Kodak Insight, the Kodak RVG-6000 and the Duerr Vistascan system. The images that were produced over a wide range of exposure factor settings were evaluated in terms of diagnostic guality by three experienced radiologists. Results: The number of images with acceptable diagnostic quality was in total 1257; 310 with Insight, 331 with RVG 6000 and 616 with Vistascan. At 60 kV, diagnosable images were produced with doses ranging from 0.44 - 1.56 mGy for the Insight film 0.44 - 2.82 mGy for the RVG 6000 and 0.22 - 4.93 mGy for the Vistascan system. At 70 kV, the respective ranges were 0.39 - 1.28 mGy for the Insight film 0.31 - 2.55 mGy for the RVG6000 and 0.30 - 3.46 mGy for the Vistascan system. Conclusions: The Vistascan exhibited the widest useful exposure range and required the least exposure to produce a diagnosable image at almost all tube potential settings. The RVG 6000 exhibited a slightly wider useful exposure range than the Insight film, with almost the same dose requirements especially in higher Kv settings.

Keywords: Radiography, Dental, Digital; Dosage

1. INTRODUCTION

According to the UNSCEAR 2000 Report, dental intraoral radiography is among the most frequently performed radiological procedures [1]. Although the patient exposure associated with dental radiography is relatively low, intraoral radiography should be optimised in order to keep the radiation risk "as low as reasonably achievable", something that is widely known as the ALARA principle [2].

Over the past 20 years both the X-ray units and the X-ray receptors used in dental radiology have been evolved. Modern dental X-ray units incorporate high frequency generators, operate at higher tube potentials and produce X-ray spectra that have higher mean energy and therefore are more penetrating compared to those produced by older dental X-ray units. These improvements have contributed in the reduction of the radiation dose to the entrance skin surface of the patient and the enhancement of image quality. Concerning the X-ray receptors, new digital systems have been introduced in to the clinical practice and nowadays digital radiography is considered an accepted imaging technique in dentistry. Currently, solid-state detectors based on CCD or CMOS technology, photostimulable storage phosphor (PSP) systems, along with the old-fashioned but still widely used silver halide based films, are commercially available for intraoral radiography.

In the international literature many remarkable articles can be found describing digital receptor systems and presenting comparisons among various systems with regard to their diagnostic performance [3-7]. Their results, however, have been derived using a limited range of exposure factors, despite the fact that the response of films and solid state or PSP receptors is dependent on the energy spectrum of the X-ray beam used and the

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dose levels to which they are exposed. The influence of the exposure factors on the performance of dental receptors of different technologies has not yet been investigated extensively.

The purpose of this study was to comparatively evaluate, in a systematic inter-equipment manner, the useful exposure range of three intraoral image receptors which are representative of the currently available technologies, when exposed to different X-ray beam spectra, dose and dose rate levels.

2. MATERIAL AND METHODS

A modern dental X-ray unit (Prostyle Intra DC, Planmeca Oy, Helsinki, Finland) was used, offering eight tube potential settings (ranging from 50 to 70 kVp), seven tube current settings (ranging from 2 - 8 mA) and 26 exposure time settings (ranging from 0.01 to 3.2 sec). The nominal total filtration was 2 mm Al and the focus to collimator end distance was 30 cm.

A calibrated ion chamber dosimeter (Dosimeter 9010, ionization chamber type 90x6-6; Radcal Corporation, Monrovia, USA) positioned at 30 cm from the tube focus was used to measure the dose in free air and determine the tube output at that distance. These measurements were carried out for all the available tube potential, tube current and exposure time selections, in order to identify possible variations in output with different tube loading values. The tube potential accuracy and reproducibility were checked using a calibrated kilovolt peak meter (Gammex RMI 245, Gammex Inc., Middleton, USA).

The intraoral radiographic receptors evaluated in this study were: the Kodak Insight F speed class film (Eastman Kodak Company, Rochester, NY), the Kodak RVG 6000 (Eastman Kodak Company, Rochester, NY), and the Duerr Vistascan Combi PSP system (Duerr Dental, Bietingsheim-Bissingen, Germany). The main technical characteristics of the systems tested are summarized in **Table 1**.

A cylindrical Perspex based phantom (Dental Image Quality Test Tool, model 76025; Nuclear Associates, Division of Victoreen, Inc, Carle Place, NY) was used for the evaluation of image quality [8]. This phantom contains a real human tooth in the centre and around it three cylindrical air filled holes of different height. In the periphery of the phantom four wire meshes of different wire thickness are included. Finally, the phantom has a slot in order to fit in the various image receptors. A photograph and a radiographic image of the phantom are shown in **Figure 1** and **Figure 2**, respectively.

The phantom was attached to the collimator end and the image to receptor distance was kept constant at 35 cm. The phantom was radiographed using all the image receptors and for each receptor all the tube potential, tube current and exposure time combinations possible. Thus, 1456 exposures were required for each image receptor in total.

The films were processed immediately after exposure, with an automatic processor (Velopex Extra-X, Medivance Instuments, England) using the Readymatic dental developer and Readymatic dental fixer solutions (Eastman Kodak, Rochester NY), at a temperature of 27°C. This processor features an automatic replenishment system, however, in order to ensure that the processing conditions remain fairly constant during the experiments, the processing stability was repeatedly tested every 50 films using sensitometry (Pehamed densitometer Densinorm 21, PEHA med. Geräte GmbH Sulzbach, Germany). The acquired film radiographs were mounted in opaque plastic holders and coded for later use. The film radiographs were evaluated on a viewing box, with all extraneous light masked.

For the Vistascan the PSP image plates were unpacked in a dimly lit room and scanned immediately after exposure, using the Vistascan Combi system [9,10]. The scanner's resolution pitch settings were adjusted to 12.5 μ m (corresponding to a theoretical resolution of 40 line pairs per mm). Concerning the RVG 6000 the original software of the system was used for image capture. No image processing was performed to enhance image quality other than the system's default pre-process.

All digital images were viewed in fit to screen mode

| Model | Manufacturer | Pixel Size (µm) | Technology | Software | Size | Bit/Pixel | Width (Pixel) | Height (Pixel) | File Size (MB) |
|---------------|--------------|--------------------|------------------|---------------------------|------|-----------|------------------|-------------------|-------------------|
| INSIGHT | KODAK | N/A | SILVER HALIDE | N/A | 2 | N/A | 3.1 (cm) | 4.1 (cm) | N/A |
| RVG 6000 | KODAK | 18.5 × 18.5 | CMOS | KODAK WINDOWS 6.0.1 | 1 | 8 | 1200 | 1600 | 1.8 |
| PSP VISTASCAN | DUERR | SCAN PITCH 12.5 | IMAGE PLATE | DBSWIN V.3.3 | 2 | 16 | 2476 | 3195 | Up to 9.3 |

Table 1. Specifications of the systems.

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Figure 1. Photograph of the phantom used for the evaluation of image quality.



Figure 2. Radiographic image of the phantom used for the evaluation image quality.

on a 19-inch TFT monitor (Sony SDMHS95PR), with 1280×1024 resolution under subdued lighting conditions. The monitor's brightness and contrast were adjusted using the SMPTE (Society of Motion Picture and Television Engineers) test pattern [11,12].

All the images acquired were evaluated by three experienced radiologists in the department of Oral Diagnosis and Radiology of the Dental School of the University of Athens. For each image, the observers evaluated the cementoenamel junction, the dentoenamel junction, the root canals and the apical region of the tooth, as well as, the perceptibility of the three holes and the four wire-mesh areas included in the phantom. An image was considered to have adequate diagnostic quality when all the aforementioned anatomical characteristics of the tooth were properly imaged and additionally the holes and the wire meshes were discernible. It had been decided that in case of disagreement among the observers, the images in question would be reviewed for a second time and if disagreements were not resolved, the opinion of the majority would be adopted.

3. RESULTS

The output measurements revealed that the linearity of

output was within accepted limits at all tube potentials, even though for small tube loadings (≤ 0.5 mAs) a reduction in output of up to 20% was observed with respect to the mean value of output over the whole mAs range. The reproducibility of output using the same exposure conditions was found to be better than 1%. The tube potential accuracy and reproducibility were found better than 3% and 1%, respectively.

For all the images of acceptable quality, the receptor type, the exposure factors (kV, mA, s) were noted and the respective entrance surface air kerma (ESAK) values at the phantom were then assigned. Examples of such images derived for a given combination of tube potential and tube current and varying exposure time, are embedded in **Table 2**, which is indicative of the differences observed among receptors with respect to their useful exposure range.

Concerning the images of insufficient quality that were considered non-diagnosable, these included the under and over exposed films and those digital images in which the appearance of the phantom resembled those of over or under exposed films, as well as, digital images with excessive noise or other artifacts (partial inversion of the greyscale in parts of the image, blooming effects etc).

The number of images with acceptable diagnostic quality was in total 1257; 310 with Insight, 331 with RVG 6000 and 616 with Vistascan. An overview of the useful exposure range of all receptors is presented (Figure 3). In this figure the exposure range of each receptor is presented with respect to the nominal mAs (left side) and the ESAK (right side), for all tube potential settings. For reasons of straightforward comparison among receptors in all insert figures the same axis scale was used. From Figure 3, it is obvious that the VistaScan PSP system exhibited by far the most extended useful exposure range for all the tube potential values used. Furthermore, it required the least dose to produce a diagnosable image at all tube potentials except 50 and 55 kV, where the Insight film required less and exactly the same ESAK, respectively. The second wider useful exposure range was exhibited by the RVG 6000. However, it required a slightly higher minimum ESAK to produce a diagnosable image compared to the Insight film, except from 60 and 70 kV where the RVG 6000 required exactly the same and less dose, respectively. The Insight film exhibited a relatively limited useful exposure range but in terms of the minimum ESAK required to produce a diagnosable image, it was the second after the Vistascan. Indicatively at 60 kV the useful exposure ranges of the VistaScan PSP, RVG 6000, Insight and were 0.22 - 4.93, 0.44 - 2.82 and 0.44 - 1.56 mGy, respectively. At 70 kV, the respective ranges 0.30 - 3.46 mGy, 0.31 - 2.55 mGy



Table 2. Images with satisfactory image quality obtained at 70 kV and 4mA with the three different receptors. The exposure time and the respective ESAK are given in the bottom rows.

Figure 3. The useful exposure range of the three receptors studied is given for all tube.

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and 0.39 - 1.28 mGy.

One may notice that a discrepancy exists among the width of useful exposure ranges of Insight film and the RVG 6000 as shown in **Figure 3** and the respective number of diagnosable images mentioned above. This is due to the fact that RVG 6000 exhibited a dependency on the dose rate, since for a specific tube potential setting and different mA selections, the same ESAK sometimes produced a diagnosable image and sometimes a non-diagnosable image. This can be seen in **Figure 4** where the useful exposure range is given for each tube loading setting separately, for tube potentials settings of 60 and 70 kV, which are the most frequently tube potential settings encountered in modern X-ray units. In this figure it can be seen that RVG 6000 exhibited a better response at low dose rates (*i.e.* lower mA settings).

Concerning the images of insufficient quality, these included the under and over exposed films and those digital images in which the appearance of the phantom was resembling this of over or under exposed films and images with excessive noise and artifacts. Some characteristic examples of the non diagnosable images and error images obtained with the three receptors have been gathered in **Figures 5(a)** to 5(h).

It can be seen that while in **Figure 5(a)** the appearance of the digital image obtained with the RVG 6000 receptor was similar to that of an overexposed film, further increase of the exposure time produced the noisy image of **Figure 5(b)**, in which the greyscale was automatically inverted. A similar situation is presented in **Figures 5(c)** to **5(e)**. With tube potential and tube current constant, starting from a digital image that was looking like an overexposed film (**Figure 5(c)**), further increase of the exposure time produced initially an image that was almost black (**Figure 5(d)**) and then an image where the phantom structures reappeared to some extent but with inverted greyscale (**Figure 5(e)**).

In **Figures 5(f)** and **5(g)** the appearance of an underexposed and an overexposed image with the Vistascan receptor, respectively, are shown. Finally, in **Figure 5(h)**



Figure 4. The useful exposure range of the three receptors studied is given for each one of the tube current settings used, for a tube loading of 60 (left figure's side) and 70 kV (right figure's side). Each diagnosable image is represented by a data point.

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(e) (f) (g) (h) **Figure 5.** Examples of images that were rejected due to lack of image quality and error images that when the exposure was repeated they resulted in diagnosable images. Rejected images with the RVG 6000 receptor; (a) 50 kV, 8 mA, 1.6 sec, (b) 50 kV, 8 mA, 2.5 sec, (c) 63 kV, 8mA, 0.64 sec, (d) 63 kV, 8mA, 0.8 sec, (e) 63 kV, 8mA, 1.6 sec. Vistascan (f) - (g), f) 70 kV, 8mA, 0.01 sec (g) 70 kV, 3mA, 3.2 sec, (h) 55 kV, 8mA, 0.01 sec. Error images with the RVG 6000 (k) receptor.

an error with the RVG 6000 receptors is shown. This error was attributed to some kind of "fatigue" that the detectors may have experienced during successive exposures.

4. DISCUSSION

Diagnosable image refers to a quality radiograph in which the examined anatomic structure is captured with fidelity. Image quality describes the subjective judgment by the clinician of the overall appearance of a radiograph. It combines the features of density, contrast, latitude, sharpness, resolution and perhaps other parameters. Various mathematical approaches have been used to evaluate these parameters further, such the detective quantum efficiency (DQE) that encompasses image contrast, blur, speed and noise. Often a system can be optimized for one of these parameters, but this is usually achieved at the expense of others. However, more information is needed for complete understanding of all the factors responsible for the subjective impression of image quality. Three main factors that control quality are receptor characteristics, geometric factors and subject characteristics.

The wide exposure range of the storage phosphor technology receptors, well known from their applications in general radiology, has been also confirmed in the dental field [13-17]. The phosphor plate systems can accommodate exposure times which are close to or at the end of the electronic timer range of many commercially available X-ray units. Since the radiographs from the Vistascan receptor remained diagnosable from very low to very high values of tube loading for all tube potential values, no re-takes will be normally needed when this type of receptor is used. On the other hand, it is also true that with receptors of this type, higher doses than those actually needed for diagnosis can be systematically used, something that from the aspect of radiation protection is considered disadvantageous and in general radiology it has been reported as "the exposure factor creep" [18].

Concerning the minimum exposure that could give a diagnosable image, as it can be seen in **Figure 3**, differences were observed among the three receptors tested, especially for the lower kV settings used. However, for the larger tube potential settings these differences were quite smaller. At 70 kV the minimum required ESAK value was about 0.3 mGy for the Vistascan and the RVG 6000, and about 0.4 mGy for the Insight. Regarding the variation of the minimum ESAK required to produce diagnosable images with the different tube potential settings, the smallest variations were observed for Insight (0.35 - 0.44 mGy) and the Vistascan (0.31 - 0.48 mGy).

The manufacturers of digital radiographic systems of-

ten claim that their systems offer a reduction in patient exposure when compared to films. In the literature it is also generally accepted that the patient dose is generally lower in digital than in conventional film based intraoral radiography with films of E-speed class [19-21]. However, in this study only the Vistascan produced diagnosable images at lower doses than the Insight film in all tube potentials except at 50 kV, where it required more dose and at 55 kV where it required exactly the same dose.

The dependence of the response of RVG 6000 on the dose rate was another interesting finding of this study. The limitation of the useful exposure range of the RVG 6000 observed with the increase of tube current settings, could be in part attributed to the difficulty of the receptor controlling, in a linear and reproducible way, the extremely short exposure times.

European guidelines, in the context of the ALARA principle, have recommended the establishment of diagnostic reference levels (DRLs) in dental radiography [22]. Relevant surveys conducted in Greek dental radiographic facilities over the last 10 years have demonstrated a trend for reduction of the entrance surface dose [8,23]. Hatziioannou *et al.* had suggested a DRL of 3.5 mGy for the intraoral dental equipment operating in Greece [24]. However, in a recent study Gonzalez *et al.*, have suggested a reference value of 1.8 mGy for E/F speed class films and 0.6 mGy for the digital image receptors [25].

In this study it was shown that for the specific phantom used, the Kodak Insight F speed class film required doses quite smaller than the typical value suggested by Gonzalez *et al.* [25] to produce images of satisfactory diagnostic quality. On the other hand, regarding the digital receptors the entrance dose of 0.6 mGy proposed by Gonzalez *et al.* was outside the lower limit of the useful exposure range of the RVG 6000 at tube potentials of 50, 55 and 57 kV [25]. It is therefore obvious that since the minimum dose required is strongly dependent on the tube potential selection, any reference or DRL values should also specify the tube potential range to which they apply.

Since the vast majority of the dental X-ray units of those commercially available and those currently in use worldwide, offer a single or at best two tube potential or tube current settings, it should not be taken for granted that these are compatible with all commercially available digital receptors.

Most modern dental X-ray units operate at a tube potential value in the range of 60 to 70 kV. However, many of them have only one tube current value setting that is usually 7 mA and therefore, if combined with a digital receptor of limited exposure range, only the very short exposure time settings in the range of 0.1 to 0.3 sec could be utilized for tube potentials larger than 60 kV (assuming that these X-ray units have an output and a total filtration similar to that of the unit used in this study and that the same focus to receptor distance is used). This problem will be more pronounced in dental X-ray units with shorter collimators offering a minimum focus to skin distance of about 20 cm (which is the case for the majority of dental X-ray units), where only two or three exposure time selections smaller or equal to 0.1 sec may be available for producing a diagnosable image. However, in X-ray units which offer a tube current around 4 mA as the standard or as an alternative selection, a wider range of exposure time settings can be utilized.

The differences observed in the useful exposure range of the receptors tested, suggest that manufacturers should include in the technical data sheets relevant information concerning the useful exposure range of their receptors in terms of tube potential, ESAK and ESAK rate in reference to a dental phantom (like this used or any other that could serve as a reference dental phantom). In this way the potential user would be able to determine if a given receptor is compatible with the dental X-ray unit that may already have and furthermore he/she would be able to compare receptors using a performance index that relates to the clinical practice and therefore is easy to comprehend.

5. CONCLUSIONS

In conclusion, Vistascan presented the widest useful exposure range compared to the RVG 6000 and the Insight film. At almost all tube potentials Vistascan required the least dose to produce a diagnosable image, something that clearly is an advantage. On the other hand, Vistascan could produce diagnosable image with doses twice or three times the upper limit of the useful exposure range of the RVG 6000 and the Insight, something that in the hands of an untrained dentist may become a serious disadvantage. RVG 6000 exhibited a wider useful exposure range than the Insight film with almost the same dose requirements especially in higher Kv settings.

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